PERKAT RV: first in vivo data of a novel right heart assist device



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KEYWORDS

- femoral
- miscellaneous
- ventricular assist device

Abstract

Aims: Mechanical right ventricular (RV) support offers a treatment option for critically ill patients with RV failure (RVF). We developed an assist device for rapid percutaneous implantation. The aim of the present study was to investigate the implantation procedure, haemodynamic performance and possible side effects of the novel right ventricular assist device - PERKAT RV - in an animal model.

Methods and results: The PERkutane KATheterpumptechnologie RV (PERKAT RV) device consists of a nitinol chamber covered by foil containing inflow valves. An outlet tube is attached to its distal part. The system is designed for 18 Fr percutaneous implantation. The chamber is unfolded in the inferior vena cava while the outlet tube bypasses the right heart with the tip in the pulmonary trunk. An IABP balloon is placed inside. Balloon deflation generates blood flow into the chamber; during inflation, blood is guided into the pulmonary arteries. Acute RVF was induced by venous injection of Sephadex in seven sheep for evaluation of the device. The PERKAT RV was able to improve haemodynamics immediately generating a median increase in cardiac output of 59%. Longer pump support was evaluated in a second study. Four sheep were supported for eight hours without any problems.

Conclusions: The percutaneous implantation and explantation of the PERKAT RV device was possible in the designed way. The sheep studies proved beneficial haemodynamic effects in acute RVF. The system offers easy and safe treatment in acute RVF.

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Abbreviations

activated clotting time
electrocardiogram
extracorporeal membrane oxygenation
French
intra-aortic balloon pump
inferior vena cava
pulse contour cardiac output
right percutaneous
right ventricle
right ventricular assist device
right ventricular failure

Introduction

Right ventricular failure (RVF) is still a clinically unsolved problem. The predominant causes of RVF are acute pulmonary embolism, left-sided heart failure, and myocardial infarction. The in-hospital mortality of patients with RVF ranges from 6-17%^{1,2}.

The clinical management of RVF is based on reversal of the underlying cause, volume optimisation to increase RV preload, vasopressor and inotropic support to stabilise haemodynamics, and pulmonary vasodilatation to reduce RV afterload. Acute mechanical circulatory support of the right ventricle should be discussed in cases of profound RVF³. Besides surgically implantable right ventricular assist devices (RVADs), percutaneously delivered circulatory support in RVF is an increasing field with only a few devices presently available. The well-established systems such as veno-arterial extracorporeal membrane oxygenation (ECMO), the TandemHeart (CardiacAssist, Inc., Pittsburgh, PA, USA)⁴, or the Impella RP[®] (Abiomed Inc., Danvers, MA, USA)⁵ show certain limitations. We therefore

developed a new percutaneously implantable RVAD - PERKAT[®] RV. The technical dossier and *in vitro* performance were published recently^{6,7}. The system is based on a nitinol stent which has to be implanted into the inferior vena cava via an 18 Fr approach and uses the already established intra-aortic balloon pump (IABP) system as its drive unit. In standardised *in vitro* evaluation, the PERKAT RV device was able to provide circulatory support of up to 3.9 L/min.

The aim of the present study was to investigate the implantation procedure, haemodynamic performance and possible side effects of the novel right ventricular assist device - the PERKAT RV - in an animal model.

Methods

PERKAT RV

The concept, technical dossier, and implantation technique of the PERKAT RV system were published recently^{6,7}.

In brief, the 18 Fr PERKAT RV system consists of a 220 mm nitinol stent cage which is covered by flexible membranes containing foil valves. A flexible outlet trunk with a pigtail tip with outflow valves is attached to the distal part of the stent cage. A standard IABP balloon is placed inside the stent and connected to a standard IABP console as the power unit for the PERKAT RV. Deflation of the IABP generates a slight negative pressure causing blood flow into the stent cage through the foil valves. During balloon inflation, the foil valves will be closed due to the pressure created by the helium-filled IABP balloon. This creates a pulsatile blood flow through the flexible outlet tube towards the pigtail ending. The novel foil valve concept enables a given direction of blood flow. The PERKAT RV is designed for percutaneous sheathless implantation (Figure 1).



Figure 1. Schematic drawing of the PERKAT RV.

ANIMALS

Adult female sheep (15 Merino animals; two to six years old [3.64 ± 0.34 years, mean \pm SEM]; 55-85 kg body weight [69.33 ± 2.55 kg]) were used. Permission for the animal experiments was obtained from the governmental commission for animal protection, Free State of Thuringia, Germany (registration number: 02-048/14). All animals received appropriate care in compliance with the "Principles of Laboratory Animal Care" formulated by the National Society for Medical Research and the "Guide for the Care and Use of Laboratory Animals" prepared by the Institute of Laboratory Animal Resources and published by the National Institutes of Health (NIH Publication No. 86-23, revised 1996).

ANAESTHESIA AND SURGICAL TECHNIQUE

After food withdrawal for 24 hrs, anaesthesia was induced by intramuscular injection of 10-15 mg·kg⁻¹ ketamine (Ketavet[®]; CP-Pharma, Burgdorf, Germany) and 0.2 mg·kg⁻¹ midazolam (Midazolam-Hameln[®]; Hameln Pharmaceuticals, Hamelin, Germany). Following orotracheal intubation, an inhalation anaesthesia was induced (isofluorane 1.5-1.8 vol% [Isofluran-CP[®]; CP-Pharma], propofol 0.2 mg/kg/hr i.v. [Narcofol 10 mg/ml; CP-Pharma]). Perioperative analgesia was induced by intravenous injection of 0.1 mg/kg fentanyl before the operation (Fentadon[®]; Albrecht GmbH, Aulendorf, Germany). A venous catheter was implanted in both jugular veins for intraoperative administration of analgesics and volume substitution, which was performed by supply of Ringer's lactate solution (10 ml/kg/hr) (Fresenius Kabi Deutschland GmbH, Langenhagen, Germany). Analgesics (0.1 mg/kg fentanyl [Fentadon]) were administered upon need or hourly.

All sheep were additionally instrumented with vascular sheaths inserted into both femoral arteries for blood sampling and blood pressure measurement and into both femoral veins (Radifocus[®] Introducer II, 6 Fr/7 Fr; Terumo, Tokyo, Japan) for implantation of the PERKAT RV. Arterial and venous blood pressure was recorded using transducers (Combitrans Transducer[®]; Braun, Melsungen, Germany).

Electrocardiograms (ECG) were derived using cutaneous adhesive electrodes. Heparin (70 IU/kg bw; Rotexmedica GmbH, Trittau, Germany) was administered intravenously before starting the procedure.

Blood gases and lactate were measured once per hour on a standard clinical blood gas analyser (ABL 600; Radiometer GmbH, Willich, Germany).

After the experiment, animals were euthanised by intravenous injection of pentobarbital sodium (Narcoren[®]; Merial, Hallbergmoos, Germany).

IMPLANTATION PROCEDURE

After the animals were anaesthetised, the femoral vessels on both sides were provided with sheaths (6 Fr for the arteries and 7 Fr for the veins) using the percutaneous Seldinger technique. Then, 5,000 IU of heparin were intravenously administered. Via both femoral veins, two 5 Fr standard pigtail catheters (Boston Scientific,

Marlborough, MA, USA) were placed in the pulmonary trunk using a standard 0.035-inch J-tip wire (EMERALD® PTFE guidewire; Cordis, Cardinal Health, Milpitas, CA, USA). The first catheter was used for monitoring pulmonary artery pressure and application of Sephadex® (if indicated) (Sigma-Aldrich, St. Louis, MS, USA). The second pigtail catheter was used to insert a super stiff 0.035-inch wire (Amplatz Super Stiff[™]; Boston Scientific). After the placement of the super stiff wire, the sheath was removed and the femoral vein access dilated using 16, 18, 20, and 22 Fr dilators (Cook Medical, Bloomington, IN, USA). The flushed PERKAT RV device was then inserted, and the pumping chamber deployed in the inferior vena cava using fluoroscopy guidance (Figure 2). After removing the super stiff wire, a standard IABP balloon (34 cc Sensation; Maquet Getinge Group, Rastatt, Germany) was inserted into the pumping chamber of the PERKAT RV pump and connected to a standard IABP console (Datascope System 97; Maguet Getinge Group) and the pump support was launched. Another 5,000 IU of heparin were administered and a 500 ml infusion of sodium chloride 0.9% with 7,500 IU of heparin was connected to the side port of the system and started with a speed of 125 ml/hr. We aimed for an activated clotting time (ACT) of more than 250 seconds.

Resting haemodynamics were measured before PERKAT RV implantation and then every 30 to 60 minutes.



Figure 2. Positioning of the PERKAT RV in the inferior vena cava of a sheep.

INDUCTION OF PULMONARY EMBOLISM

In order to investigate the PERKAT RV in haemodynamically compromised animals, a pulmonary embolism was induced.

Macroscopic beads synthetically derived from the polysaccharide dextran (Sephadex, size 100 μ m) were dissolved in sodium chloride 0.9% (0.5 g Sephadex in 50 ml sodium chloride 0.9%); 10 ml of this solution were injected into the pulmonary trunk via a pigtail catheter. After each application, haemodynamics were measured. We defined "haemodynamically compromised" as sheep with a cardiac output <2.5 L/min and/or with a reduction of at least 50% in comparison to the initial value.

8-HOUR EXPERIMENT

To study the device for a longer time period, it was implanted in healthy sheep without induction of a pulmonary embolism. Haemodynamics were again monitored before PERKAT RV implantation and then every 60 minutes. After eight hours the device was explanted and screened for possible thrombus formation. The animals were then sacrificed.

HAEMODYNAMICS

In order to study the haemodynamic effects of the PERKAT RV, detailed haemodynamic measurements were performed. We recorded invasive blood pressure, heart rate, mean pulmonary pressure, and cardiac output at the start, after each Sephadex injection, and at the end of each experiment. In the eight-hour evaluation of the PERKAT RV, these parameters were recorded at the beginning, after device implantation, and every 60 minutes. Cardiac output was measured using the pulse contour cardiac output (PiCCO) method. For each parameter we registered three consecutive values.

LABORATORY EVALUATION

To evaluate the haemolytic potential of the PERKAT RV, blood was drawn before implantation of the device and at the end of every experiment. We measured the following parameters: haemo-globin, free haemoglobin, lactate, lactate dehydrogenase (LDH), potassium, and thrombocytes.

Results

SHEEP EXPERIMENT

The first three animals were used to study the handling, usability and functionality as well as the implantation procedure of the PERKAT RV and to establish the artificial induction of the pulmonary embolism.

PULMONARY EMBOLISM

The PERKAT RV was studied in eight sheep with acute right ventricular failure due to severe pulmonary embolism. One animal died after a Sephadex injection due to ongoing ventricular fibrillation. The PERKAT RV was therefore not implanted in this sheep. In the other seven animals, the system could be implanted without any difficulties within a few minutes. The initial cardiac output in these sheep was 4.7 L/min (\pm 0.9 L/min); after the induction of pulmonary embolism, cardiac output decreased to 2.2 L/min (\pm 0.9 L/min). The PERKAT RV was able to stabilise the animals with an increase of



Figure 3. Cardiac output (L/min) of seven sheep at baseline, after induction of pulmonary embolism, and after stabilisation with the PERKAT RV. Values are given as mean±SD.

Table 1. Cardiac output, mean blood pressure, heart rate, and
mean pulmonary artery pressure at the start, after induction of
pulmonary embolism, and during PERKAT RV support.

	Cardiac output (L/min)	Blood pressure mean (mmHg)	Heart rate (bpm)	PAP mean (mmHg)
Initial	4.7±0.9	121±12	111±13	23±4
Pulmonary embolism	2.2±0.9	56±25	104±15	40±14
PERKAT RV support	3.5±1.0	80±23	116±14	40±14
Values are given as mean+SD.				

8-HOUR EXPERIMENT

We were able to implant the PERKAT RV in all four animals without any complications. Haemodynamics remained stable over the whole period of eight hours **(Table 2)**. The slight drop in mean blood pressure was caused by the intensification of the anaesthesia by the veterinary surgeon. The other parameters (cardiac output, heart rate, mean PA pressure) remained stable.

At the end of the experiment, the system was removed without any complications. Only very small thrombi were detected on the surface of the PERKAT RV (Figure 4).

LABORATORY EVALUATION

Laboratory values of the acute and 8-hour experiment are shown in **Table 3** and **Table 4**. In the acute setting, lactate was significantly higher at the end of the experiment. The other parameters were comparable between the two measurements. There was a trend towards higher LDH and lower platelets during circulatory support with the PERKAT RV in the 8-hour setting.

Table 2. Cardiac output, mean blood pressure, heart rate, and mean pulmonary artery pressure at the start, after implantation of the PERKAT RV (0 hrs), and after 1-8 hours.

	Cardiac output (L/min)	Blood pressure mean (mmHg)	Heart rate (bpm)	PAP mean (mmHg)
Initial	6.6±0.7	105±10	116±9	21±3
0 hrs	5.4±0.7	90±16	110±13	19±4
1 hr	4.7±1.2	85±17	110±18	19±3
2 hrs	5.6±1.0	87±11	109±12	23±5
3 hrs	6.2±1.1	83±3	108±8	23±5
4 hrs	5.8±1.4	72±3	104±7	23±5
5 hrs	6.2±1.7	71±14	107±3	24±6
6 hrs	6.0±1.2	67±8	105±6	24±5
7 hrs	5.7±0.7	64±5	104±8	23±3
8 hrs	6.1±1.0	71±13	103±5	24±3
Values are given as mean±SD.				

Table 3. Haemoglobin, free haemoglobin, haematocrit, lactate dehydrogenase, lactate, potassium, and thrombocytes at the start and after 8-hour device support.

	Initial	After 8 hrs	<i>p</i> -value
Haemoglobin (mmol/L)	4.3±0.6	4.7±0.9	n.s.
Free haemoglobin (µmol/L)	11.7±6.9	18.4±9.5	n.s.
Haematocrit (%)	21±6	23±8	n.s.
Lactate dehydrogenase (µmol/L*s)	6.7±2.0	11.1±2.7	n.s.
Lactate (mmol/L)	2.1±0.8	4.5±2.6	n.s.
Potassium (mmol/L)	3.5±0.2	4.0±0.5	n.s.
Thrombocytes (Gpt/L)	180±48	119±39	n.s.
Values are given as mean±SD. n.s.: not significant			

Table 4. Haemoglobin, free haemoglobin, haematocrit, lactate dehydrogenase, lactate, potassium, and thrombocytes at the start and after induction of pulmonary embolism and device support.

	Initial	End	<i>p</i> -value
Haemoglobin (mmol/L)	4.4±0.3	5.1±0.9	n.s.
Free haemoglobin (µmol/L)	25.7±15	24.9±15	n.s.
Haematocrit (%)	21±3	26±7	n.s.
Lactate dehydrogenase (µmol/L*s)	7.2±1.0	7.0±0.7	n.s.
Lactate (mmol/L)	1.5±0.4	5.2±2.5	0.003
Potassium (mmol/L)	4.1±1.4	4.0±0.4	n.s.
Thrombocytes (Gpt/L)	118±36	97.0±32	n.s.
Values are given as mean±SD. n.s.: not significant			

period of 8 hours.

Discussion

In the present study we could prove that the percutaneous implantation and explantation procedure of the PERKAT RV was successful in terms of functionality and usability. Furthermore, the device was able to stabilise haemodynamically impaired sheep in a setting of acute pulmonary embolism. This was measured as an increase in cardiac output of 59%. In addition, the PERKAT RV was used for eight hours without any complications in four sheep.

Severe RVF is an increasing clinical problem and leads to a rise in morbidity and mortality. In the case of profound RVF, surgically implantable assist devices have been used as a last resort therapy. However, these devices involve the risks of haemolysis, thromboembolic events, and infection. In addition, outcome results of surgical RVADs are inconclusive8. Percutaneously implantable RVADs are therefore a reasonable treatment option. There are only a few systems on the market at the moment such as the Impella RP9 and the TandemHeart¹⁰. In comparison to the TandemHeart, the PERKAT RV is implantable using only one femoral vein without the need for arterial access. The PERKAT RV requires an 18 Fr access whereas the TandemHeart needs two 21 Fr cannulas¹⁰ and the Impella RP⁵ is designed to be implanted via a 23 Fr sheath. After induction of the pulmonary embolism in sheep, cardiac output went down to 2.2 L/min. The PERKAT RV system was able to stabilise these severely impaired animals haemodynamically and the cardiac output increased to 3.5 L/min. This is comparable to the findings of the RECOVER RIGHT study where the Impella RP system improved haemodynamics in a range from 1.8-3.3 L/min/m² 9. The TandemHeart system was able to increase the cardiac index by 0.5 L/min/m²¹⁰. Besides the benefits in haemodynamics, the safety issues of RVADs have to be studied. We saw one mild groin bleeding but could not detect any severe bleedings. The haemoglobin values remained stable over the whole experiment. In contrast to our results, the Impella RP was associated with 60% major bleeding events9. Kapur et al10 reported a statistically significant drop in haemoglobin of 1.4 g/dL and a major bleeding rate of 41% in the percutaneous group. However, due to the fact that all sheep in our study were sacrificed at the end of the experiment, these data have to be compared with caution. We cannot exclude that bleeding would have occurred after device explantation to some degree. Furthermore, we measured a trend towards a slight decrease in thrombocytes in the 11 reported animals. This is in concordance with the TandemHeart system where a significant drop in thrombocytes was reported¹⁰. The authors of the RECOVER RIGHT study



Figure 4. The PERKAT RV stent system after an in vivo pumping

reported a haemolysis rate of 13.3%⁹. The clinical relevance of this issue is still unclear. Again, the comparability of our data to both clinical trials is limited. The coagulation system of sheep differs significantly from that of humans¹¹.

Study limitations

The data reported in this study were collected in a small number of animals, seven sheep in the acute and four sheep in the so-called "8-hour" experiments. Further evaluation of the system in sheep is ongoing. In addition, there are several reasons for severe RVF, as discussed above. We evaluated the PERKAT RV system in this reported study in the context of acute pulmonary embolism.

Conclusions

In this paper we present the first *in vivo* evaluation of the PERKAT RV system. The handling and usability of the PERKAT RV during percutaneous implantation and explantation were demonstrated. After initiation of pump support, the PERKAT RV led to a significant increase in cardiac output in haemodynamically severely impaired sheep. Based on these findings, further research and work should now focus on implementing the results for application in human patients in the future.

Impact on daily practice

The PERKAT RV is a novel percutaneous right ventricular assist device. It offers sufficient haemodynamic support in haemodynamically impaired sheep. We therefore believe that the PERKAT RV could be a potential treatment option for haemodynamically compromised patients with right heart failure.

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Conflict of interest statement

M.W. Ferrari is co-founder and a shareholder in NovaPump. The other authors have no conflicts of interest to declare.

References

1. Maggioni AP, Dahlström U, Filippatos G, Chioncel O, Leiro MC, Drozdz J, Fruhwald F, Gullestad L, Logeart D, Metra M,

Parissis J, Persson H, Ponikowski P, Rauchhaus M, Voors A, Nielsen OW, Zannad F, Tavazzi L; Heart Failure Association of ESC (HFA). EURObservational Research Programme: the Heart Failure Pilot Survey (ESC-HF Pilot). *Eur J Heart Fail*. 2010;12: 1076-84.

2. Spinar J, Parenica J, Vitovec J, Widimsky P, Linhart A, Fedorco M, Malek F, Cihalik C, Spinarová L, Miklik R, Felsoci M, Bambuch M, Dusek L, Jarkovsky J. Baseline characteristics and hospital mortality in the Acute Heart Failure Database (AHEAD) Main registry. *Crit Care*. 2011;15:R291.

3. Harjola VP, Mebazaa A, Čelutkienė J, Bettex D, Bueno H, Chioncel O, Crespo-Leiro MG, Falk V, Filippatos G, Gibbs S, Leite-Moreira A, Lassus J, Masip J, Mueller C, Mullens W, Naeije R, Nordegraaf AV, Parissis J, Riley JP, Ristic A, Rosano G, Rudiger A, Ruschitzka F, Seferovic P, Sztrymf B, Vieillard-Baron A, Yilmaz MB, Konstantinides S. Contemporary management of acute right ventricular failure: a statement from the Heart Failure Association and the Working Group on Pulmonary Circulation and Right Ventricular Function of the European Society of Cardiology. *Eur J Heart Fail.* 2016;18:226-41.

4. Kapur NK, Paruchuri V, Korabathina R, Al-Mohammdi R, Mudd JO, Prutkin J, Esposito M, Shah A, Kiernan MS, Sech C, Pham DT, Konstam MA, Denofrio D. Effects of a percutaneous mechanical circulatory support device for medically refractory right ventricular failure. *J Heart Lung Transplant.* 2011;30: 1360-7.

5. Cheung AW, White CW, Davis MK, Freed DH. Short-term mechanical circulatory support for recovery from acute right ventricular failure: clinical outcomes. *J Heart Lung Transplant.* 2014;33: 794-9.

6. Kretzschmar D, Lauten A, Ferrari MW. In vitro evaluation of a novel pulsatile right heart assist device - the PERKAT system. *Int J Artif Organs*. 2015;38:537-41.

7. Kretzschmar D, Schulze PC, Ferrari MW. Hemodynamic Performance of a Novel Right Ventricular Assist Device (PERKAT). *ASAIO J.* 2017;63:123-7.

8. Goldstein JA, Kern MJ. Percutaneous mechanical support for the failing right heart. *Cardiol Clin.* 2012;30:303-10.

9. Anderson MB, Goldstein J, Milano C, Morris LD, Kormos RL, Bhama J, Kapur NK, Bansal A, Garcia J, Baker JN, Silvestry S, Holman WL, Douglas PS, O'Neill W. Benefits of a novel percutaneous ventricular assist device for right heart failure: The prospective RECOVER RIGHT study of the Impella RP device. *J Heart Lung Transplant*. 2015;34:1549-60.

10. Kapur NK, Paruchuri V, Jagannathan A, Steinberg D, Chakrabarti AK, Pinto D, Aghili N, Najjar S, Finley J, Orr NM, Tempelhof M, Mudd JO, Kiernan MS, Pham DT, DeNofrio D. Mechanical circulatory support for right ventricular failure. *JACC Heart Fail.* 2013;1:127-34.

11. Hecker JF. The Sheep as an Experimental Animal. London, Great Britain: Academic Press; 1983.