In vitro evaluation of valve-in-valve combinations using a SAPIEN XT valve implanted within PERIMOUNT and Magna Ease pericardial bioprostheses



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KEYWORDS

- aortic valve
- transcatheter aortic valve implantation (TAVI)
- valve
- valve degeneration
- valve-in-valve

Abstract

Aims: Implantation of a transcatheter heart valve to treat valve failure is an attractive option which is being used more frequently. Despite large clinical experience there is a paucity of *in vitro* data to support this treatment. Our aim was to provide *in vitro* performance data on the SAPIEN XT transcatheter heart valve implanted within two types of pericardial surgical heart valve.

Methods and results: A SAPIEN XT was implanted within multiple sizes, i.e., 21, 23, 25 of Magna Ease and explanted calcified PERIMOUNT valves. Each combination underwent *in vitro* testing according to the ISO 5840 guidance. Combinations were evaluated for embolisation and acute and long-term haemodynamic performance. All combinations met the ISO 5840 minimum requirements for effective orifice area (EOA) and regurgitant fraction at the initiation of the study, after 20 million and 200 million cycles. EOA was above 1.4 cm² for all valve combinations with Magna Ease and above 1.22 cm² with PERIMOUNT combinations. Regurgitant fraction was \leq 7% for SAPIEN XT-Magna Ease combinations and was \leq 10% for SAPIEN XT-PERIMOUNT combinations, which also met the ISO requirements. No embolisation was observed. The largest migration was 1.2 mm.

Conclusions: *In vitro* tests demonstrate excellent haemodynamic performance and durability in the six VIV combinations which are commonly seen in clinical practice.

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Abbreviations

AWT	accelerated wear testing
EOA	effective orifice area
ID	internal diameter
ISO	International Organization for Standardization
SHV	surgical heart valve
SVD	structural valve deterioration
TAVI	transcatheter aortic valve implantation
THV	transcatheter heart valve

VIV valve-in-valve

Introduction

The numbers of bioprosthetic heart valves implanted annually in the world are on the rise¹. With the lowering of the cut-off age for bioprosthetic surgical heart valve (SHV) implantation, and an ageing population, one can expect an increase in the number of SHVs experiencing structural valve deterioration (SVD)^{1,2}. Re-do operations carry an increased risk of operative mortality. The operative risk of elective re-do aortic valve surgery has been reported to range from 2%-7%, but can be greater than 30% in high-risk, nonelective patients³.

Transcatheter heart valve (THV) implantations into degenerated SHVs have been performed by an increasing number of physicians as an alternative to re-do surgery in high-risk patients and are referred to as valve-in-valve (VIV)⁴⁻¹⁰. VIV is an attractive option as it avoids a sternotomy and cardiopulmonary bypass and can potentially accelerate patient recovery and reduce length of hospital stay¹¹. A large body of experience exists on the use of the SAPIEN XT THV (SAPIEN XT) balloon-expandable valve (Edwards Lifesciences, Irvine, CA, USA) and self-expanding CoreValve[®] (Medtronic, Minneapolis, MN, USA) to treat degenerated aortic SHVs⁴⁻¹¹.

There are at least 16 different types of SHV which have been implanted in the last two decades¹²⁻¹⁴. Each SHV has a unique design, which can influence its compatibility with a given THV. Most users extrapolate information gained from transcatheter aortic valve implantation (TAVI) experience to perform a VIV procedure. This is especially true when choosing an appropriately sized THV for a given SHV^{11,12}. Although there is guidance available on sizing as well as positioning of THV, limited *in vitro* or *in vivo* animal data are available regarding haemodynamic performance and durability of the THV after a VIV procedure¹⁴⁻¹⁶. Similarly, *in vitro* data on the ability of a VIV combination to resist embolisation are sparse.

Edwards Lifesciences has been a leading manufacturer of both SHVs and THVs. This has provided a unique opportunity to assess *in vitro* performance data of the SAPIEN XT Model 9300TFX THV deployed into a Carpentier-Edwards PERIMOUNT Magna Ease Model 3300TFX (Magna Ease; Edwards Lifesciences) and explanted Carpentier-Edwards PERIMOUNT Models 2800 and 2900 (PERIMOUNT; Edwards Lifesciences). In this paper we discuss the clinically relevant findings of these tests with a focus on the ability of various VIV combinations to resist embolisation, on post-implant gradients and on long-term haemodynamic performance.

Methods

This study was conducted to evaluate the resistance to migration and 200 million cycle durability of the SAPIEN XT when deployed in a Magna Ease and explanted calcified PERIMOUNT pericardial valves under hypertensive conditions. A nominally deployed SAPIEN XT was used as a reference article. Important design characteristics of the three valve types under consideration are as follows:

CARPENTIER-EDWARDS PERIMOUNT DESIGN (MODEL 2800 AND MODEL 2900)

PERIMOUNT is one of the earlier versions of pericardial SHV intended for an intra-annular implantation in the aortic position. The sewing ring is higher than the bottom of the basal band (Figure 1A). It is made of three components: the frame, polyester sewing ring and three matched bovine pericardial leaflets. The frame has three posts with cobalt-chromium wire and basal band (solid but with multiple suture holes), which are visible under fluoroscopy.

There is no clinically significant difference between Model 2800 (intended for the US market) and Model 2900 (intended for Europe and the rest of the world).



Figure 1. Various heart valves used for the study. A) PERIMOUNT SHV. Side view and fluoroscopic appearance. Green arrow points to the basal band and red arrow points to the sewing ring, i.e., intra-annular design. B) Magna Ease. Side view and fluoroscopic appearance. Green arrow points to the basal band and red arrow points to the sewing ring, i.e., supra-annular design. Both arrows are at the same level. C) SAPIEN XT. Side view and fluoroscopic view. Blue arrow points to the nadir of the pericardial leaflets.

CARPENTIER-EDWARDS PERIMOUNT MAGNA EASE DESIGN (MODEL 3300TFX)

Magna Ease is the latest generation of pericardial SHV intended for supra-annular implantation in the aortic position. The sewing ring is at the same level as the bottom of the basal band (**Figure 1B**). It is also made of three components: the valve frame, polyester sewing ring and three matched bovine pericardial leaflets. The valve frame has three posts with cobalt-chromium wire and basal band (solid), which are visible under fluoroscopy.

SAPIEN XT DESIGN

The SAPIEN XT (**Figure 1C**) is a second-generation balloonexpandable THV with a cobalt-chromium frame. Three matched bovine pericardial leaflets, similar to those of the Magna Ease pericardial valve, are sutured within the frame.

Details of the sizes and important dimensions of all three valves are provided in **Table 1**.

Pulse duplicator hydrodynamic testing and accelerated wear testing systems are used to generate important functional data. Testing was carried out in accordance with ISO 5840 guidance for surgical heart valves. ISO 5840:2009 is applicable to all devices intended for implantation in human hearts, as a heart valve substitute. ISO 5840 specifies *in vitro* and preclinical *in vivo* testing and clinical evaluations. This International Standard also covers important hydrodynamic and durability characteristics of heart valve substitutes and imposes minimum performance requirements for heart valve substitutes where adequate scientific and/or clinical evidence exists for their justification. In 2013, the ISO committee released ISO 5840-3:2013 which is specifically for heart valve substitutes delivered by transcatheter techniques. Both ISO 5840:2009 and 5840-3:2013 were considered in this evaluation. This is explained in brief below.

Table 1. Important dimensions of valves tested.

Valve type	Label size	Outer diameter (OD) (mm)	Internal diameter (ID) (mm)	Height (mm)
SAPIEN	23	23	NA	14
XT	26	26	NA	17
	29	29	NA	19
PERI-	19	19	18	14
MOUNT	21	21	21	15
	23	23	22	16
	25	25	24	17
	27	27	26	18
	29	29	28	19
Magna	19	19	18	14
Ease	21	21	20	15
	23	23	22	16
	25	25	24	17
	27	27	26	18
	29	29	28	19

PULSE DUPLICATOR

The test and reference valves were tested using the open-loop Cardiac Valve Analyzer, pulse duplicator system (Edwards Lifesciences) (Figure 2). The pulse duplicator is used to perform hydrodynamic testing. It essentially simulates what a ventricle does and has sensors to detect pressures and flows, and has controls which allow adjustments of important parameters such as heart rate (beat rate), flow and back pressures. Thus, it provides hydrodynamic information on the fluid mechanical performance of the heart valve substitute. The pulsatile-flow testing conducted in the pulse duplicator approximates the physiological conditions of the intended device application in accordance with guidelines of the ISO 5840 standard for cardiovascular implants.

Accelerated wear testing (AWT) system

The test and reference valves were tested in the Edwards modified Dynatek M6 Heart Valve Accelerated Wear Tester. The valves were cycled at accelerated rates for a minimum of 20 million cycles at 160 mmHg peak differential closing pressure and an additional 180 million cycles at 95 mmHg peak differential closing pressure. AWT



Figure 2. Schematic diagram of the pulse duplicator circuit used for haemodynamic testing.

is used to cycle the valves rapidly to test durability but does not generate hydrodynamic performance data. Hence, typically every 50 million cycles the valves are removed from the AWT machines and then put in a pulse duplicator to assess valve function such as pressure gradients and leakage. The THV was also assessed for movement within the SHV. At 75 beats per minute, there are approximately 40 million heart beats per year. Although heart beats in a patient may not be the same as heart beats in the AWT, 20 million cycles equate to approximately six patient months if the heart beat rate was 75 beats per minute. This translates to five years for 200 million cycles.

All AWT testers were tuned to achieve full valve closure and opening as compared to the same valve observed under pulsatile flow conditions in the pulse duplicator at 5 lpm, 70 bpm, 100 mmHg mean arterial pressure, mean leakage pressure of 160 mmHg (for the first 20 million cycles), and $35\pm2\%$ aortic forward flow ratio. **Figure 3** shows an example of the tested valve opening and closing motions observed in the AWT.



Figure 3. *Examples of test sample opening and closing at the start* (*A*), *after 20 million cycles (B), and after 200 million cycles (C).*

The study was conducted in two parts:

PART A: *IN VITR*O VIV DURABILITY STUDY OF SAPIEN XT DEPLOYED IN A MAGNA EASE

This study was conducted to evaluate the resistance to migration and 200 million cycle durability of the SAPIEN XT when deployed in a Magna Ease under hypertensive conditions. Nominally deployed SAPIEN XT were used as reference articles.

To evaluate the ability of the SAPIEN XT to resist embolisation, the valve was subjected to a number of pulsatile and steady state conditions that represent extreme dislodgement pressures for the target patient population. For this study, valve embolisation was defined as the dislodgement of the SAPIEN XT from the intended and documented original position to an unintended and non-therapeutic location as defined in ISO 5840.

The VIV configurations below were used in the testing:

- 23 mm SAPIEN XT in a 21 mm Magna Ease
- 23 mm SAPIEN XT in a 23 mm Magna Ease
- 26 mm SAPIEN XT in a 25 mm Magna Ease
- Two 23 mm and one 26 mm SAPIEN XT used as controls

Five samples of each VIV configuration were tested. Tested valves were referenced by a unique identifier (ELX number) used by Edwards Lifesciences to document the valve for *in vitro* testing. All test valves were crimped on NovaFlex+ delivery systems (Edwards Lifesciences) and underwent deployment through a simulated aortic arch crossing.

Valve performance testing was conducted in accordance with the requirements of the Cardiovascular Implants - Cardiac Valve Prostheses International Standard Guidance: ISO 5840:2005 (section 7.2.3 and Annex L4). The Edwards modified Dynatek M6 AWT was used to simulate hypertensive pressures of 160 mmHg for 20 million cycles (equivalent to six months) and normotensive pressures of 95 mmHg for an additional 180 million cycles at a rate range of 1,000-1,200 bpm (beats per minute). In order to assess the impact of each test condition on migration (precursor to valve embolisation), the valves were subjected to macroscopic inspection, X-ray migration measurement, and photo documentation at each test interval (e.g., pre-pulsatile, post-normotensive pulsatile, post-steady forward flow, post-steady back-pressure, post-hypertensive pulsatile, and post-20 million cycles and at 50, 100, 150, and 200 million cycles AWT). The valves were mounted as shown in Figure 4A and Figure 4B.

STAGES OF VALVE PERFORMANCE TESTING

Pre-pulsatile means, shortly after the THV was placed inside the surgical valve, the inspections and X-rays were performed, before any testing of the valves.

Post-normotensive pulsatile means, after testing in a pulse duplicator (cardiac simulator or PD) under normotensive conditions in the aortic position, the inspections and X-rays were performed, before any testing of the test valves. This test lasts about 10 to 30 minutes depending on the ease of adjusting the machine.

Post-steady forward flow means, after testing in a non-pulsatile device where flow was stepped up from a low of 5 lpm (litres per minute) up to 30 lpm in 5 lpm increments, the inspections and



Figure 4. *Valve mounting for testing. A) Outflow view of a representative sample of VIV in a valve mount. The combination shown is 23 SAPIEN XT in a 23 Magna Ease. B) Outflow view of a representative sample of a 23 SAPIEN XT mounted in a valve mount as a control.*

X-rays were performed, before any testing of the test articles. This test lasts about 10 to 30 minutes depending on the ease of adjusting the machine.

Post-steady back flow means, after testing in a non-pulsatile device where the valve is closed and back pressure is steadily increased from 40 mmHg to 80, to 120, to 160 and to 200 mmHg, the inspections and X-rays were performed, before any testing of the test valves. This test lasts about 10 to 30 minutes depending on the ease of adjusting the machine.

Post-hypertensive pulsatile means, after testing in a pulse duplicator (cardiac simulator) under hypertensive conditions of 160 mmHg in the aortic position, the inspections and X-rays were performed, before any testing of the test valves. This test lasts about 10 to 30 minutes depending on the ease of adjusting the machine.

Post-20 million AWT means after cycling in a durability tester for 20 million cycles under hypertensive conditions of 160 mmHg in the aortic position. Note, only the first 20 million cycles in the pulse duplicator are run at pressures >160 mmHg. This test in the PD lasts about 10 to 30 minutes depending on the ease of adjusting the machine.

Subsequent testing to 200 million cycles means, after the 20 million cycle test at 160 mmHg and the inspections, the valves were put back in the durability testers and run to 200 million cycles (equivalent to five years of heart beats) and normotensive pressures exceeding 95 mmHg. At 50 million cycles and every 50 million cycles thereafter, the testers are stopped, the valves removed

and the same inspections and tests are performed before the valves go back in the tester.

At the end of 200 million cycles, we subsequently did a few pull tests on the non-explant combinations. This was not intended originally but was performed after an FDA request. We can provide these data for you if you wish.

VALVE-IN-VALVE DEPLOYMENT

DEPTH OF IMPLANT

In this study, the outflow edge of the SAPIEN XT was aligned just below the free edge of the Magna Ease leaflets. This position was determined to be an optimal placement because there is no SHV leaflet overhang and sufficient overlap between the THV frame and SHV basal band to anchor the THV securely. In **Figure 5**, a representative VIV configuration shows the vertical positioning. The percent ventricular positioning ranged from 7% to 28% for the test valves (**Table 2**). The percent ventricular positioning varies depending on the relative heights of the SHV and THV.

ORIENTATION

The orientation (commissural angle offset) for the final deployment of the SAPIEN XT in the Magna Ease was targeted to be evenly distributed between the two extremes, 0 degrees (frame post to frame post) and 60 degrees (halfway between two frame posts), with the remaining sample oriented at 30 degrees (halfway between previous two samples) (Figure 6).



Figure 5. *THV frame position within Magna Ease. A) Side view of a 23 Magna Ease with 23 SAPIEN XT frame visible through the leaflets (red arrows). Deployment was performed to align the top of the THV with the top of the leaflets of the SHV. B) Fluoroscopic view of the same combination demonstrates that 20% of the SAPIEN XT frame is below the basal band, i.e., ventricular.*

olnte	Table 2. Detailed data set of Magna Eas							
olntervention 2016;11: @1291-@1301	Combina- tion	ID no.	Surgical model	Magn Ease size				
1291-	23S-21M	17195	Magna Ease 3300	21				
e 13		17196	"	21				
01		17197	"	21				
		17198	u	21				
		17199	"	21				
	23S-23M	17207	"	23				
		17208	"	23				

se and SAPIEN XT combination.

ISO EOA minimum **ISO EOA minimum** Ratio of SAPIEN ventricu-SHV true requirement requirement 2013 a SAPIEN True ID THV lar below XT (cm²) ID/SAPIEN 2005 (cm²) (based (cm²) (based on (@ 200 (mm) model XT size the basal **XT** outer on surgical valve surgical valve stiffening million diameter size) size) band (%) cycles) SAPIEN 19 23 25 1.56 0.85 1.05 0.82 XT 19 " 23 0.82 26 1.56 " 19 23 0.82 22 1.57 " 0.82 19 23 23 1.49 " 0.82 22 1.57 19 23 " 21 0.91 1.73 1.00 1.25 23 26 " 21 23 0.91 20 1.52 " " 17209 1.77 23 21 23 0.91 15 " " 17211 23 21 23 0.91 22 1.74 " " 17212 0.91 1.7 23 21 23 7 " 26S-25M 17201 25 23 " 26 0.88 24 1.93 1.20 1.45 " " 17202 25 23 0.88 24 2.00 26 " " 17203 25 23 26 0.88 28 2.00 " " 17204 25 0.88 2.04 23 26 27 17205 " 25 23 " 26 0.88 25 2.00

EOA: effective orifice area; M: Magna Ease surgical heart valve; S: SAPIEN transcatheter heart valve

PART B: IN VITRO VIV DURABILITY STUDY OF SAPIEN XT DEPLOYED INTO EXPLANTED CALCIFIED PERIMOUNT VALVES

This study was conducted to evaluate the durability of the SAPIEN XT when deployed in an explanted PERIMOUNT valve with moderate to severe calcification. A nominally deployed SAPIEN XT was used as a reference article.

Explanted surgical valves were selected from customer returned

valves that met the criteria list below:

- Valve was stenotic and exhibited extensive calcification

- Frame was not noticeably damaged during explant

EOA after

Percent

- Sewing band was intact such that the valve could be mounted to the test fixture

Figure 7A and Figure 7B show a representative test valve mounting technique, which displays the inflow and outflow view of a size 23 mm explanted PERIMOUNT valve prior to having a 23 mm SAPIEN XT valve deployment. Figure 7C and Figure 7D



Figure 6. Orientation of the SAPIEN XT in relation to the frame posts of the SHV. A) & B) Stent post to frame post deployment – 0 degree orientation. C) & D) 30 degree orientation. E) & F) 60 degree orientation.



Figure 7. Mounting technique for an explanted calcified PERIMOUNT SHV with SAPIEN XT (sample shown is a 21 PERIMOUNT with a 23 SAPIEN XT). A) & B) Inflow and outflow of PERIMOUNT before SAPIEN XT implantation. C) & D) Inflow and outflow of VIV combination after SAPIEN XT implantation.

show the same inflow and outflow view after the VIV deployment of a size 23 mm SAPIEN XT.

SAPIEN XT implantation was carried out using the NovaFlex+ delivery system in an identical fashion to the valves in the prior section with regard to depth and orientation (Figure 8, Table 3).

The test protocol was the same as that for the valves in the prior section.

Results

PART A: *IN VITRO* VIV DURABILITY STUDY OF SAPIEN XT DEPLOYED IN A MAGNA EASE

All valves met the ISO 5840 minimum requirements, which are applicable to replacement valves, for effective orifice area (EOA) and regurgitant fraction at the initiation of the study, at the completion of 20 million cycles, and at the completion of 200 million cycles.

At 5 lpm and 70 bpm, the EOA for the 21 mm SHV – 23 mm THV VIV combinations was above 1.2 cm² for all valves, the EOA for the 23 mm SHV – 23 mm THV VIV combinations was above 1.5 cm² for all valves, and the EOA for the 25 mm SHV – 26 mm THV VIV combinations was above 1.8 cm² for all valves, which



Figure 8. *SAPIEN XT frame position within calcified explanted PERIMOUNT. A) Side view of a 23 PERIMOUNT with a 23 SAPIEN XT with the frame visible through the leaflets (red arrows). Deployment was performed to align the top of the THV with the top of the leaflets of the SHV. B) Fluoroscopic view of the same combination demonstrates that 5% of the SAPIEN XT frame is below the basal band, i.e., ventricular.*

Combi- nation	ID no.	PERI- MOUNT model	PERI- Mount size	True ID (mm)	THV model	SAPIEN XT size	Ratio of SHV true ID/ SAPIEN XT outer diameter	Percent ventricular below the basal stiffening band (%)	EOA before SAPIEN XT (cm²)	EOA after SAPIEN XT (cm ²) (@ 200 million cycles)	requirement 2005 (cm²) (based on	ISO EOA minimum requirement 2013 (cm²) (based on surgical valve size)
23S-21P	17279	2800	21	19	SAPIEN XT	23	0.82	16	0.56	1.36		1.05
	17280	2900	21	19	u	23	0.82	10	0.40	1.24	0.85	
	17281	2800	21	19	"	23	0.82	13	0.35	1.22		
23S-23P	17276	2800	23	21	"	23	0.91	9	0.59	1.61		1.25
	17277	2900	23	21	"	23	0.91	5	0.68	1.39	1.00	
	17282	2800	23	21	u	23	0.91	-3	0.84	1.55		
26S-25P	17278	2900	25	23	u	26	0.88	5	0.53	1.91		1.45
	17283	2800	25	23	"	26	0.88	11	0.65	1.94	1.20	
	17284	2800	25	23	"	26	0.88	11	0.64	1.89		
P: PERIMOU	P: PERIMOUNT surgical heart valve; S: SAPIEN transcatheter heart valve											

Table 3. Detailed data set of calcified PERIMOUNT and SAPIEN XT combination.

were above the ISO requirements of $\ge 0.85 \text{ cm}^2$ for 21 mm valves, $\ge 1.0 \text{ cm}^2$ for 23 mm valves and $\ge 1.2 \text{ cm}^2$ for 25 mm valves, respectively **(Table 2)**. Reference transcatheter valves were included in this study. At the conclusion of the study at 200 million cycles, the EOA of the 23 mm reference valves exceeded 1.6 cm² and the 26 mm reference valves exceeded 2.2 cm².

REGURGITANT FRACTION

Regurgitant fraction for all valves was \leq 7%, which met the ISO 5840 requirement of \leq 10% for 21 mm and 23 mm valves and \leq 15% for 25 mm valves, both initially and at 200 million cycles. **AWT DURABILITY TEST**

The test and reference valves remained competent through 200 million cycles. All valves were able to maintain target peak differential closing pressures. No valve was removed from the study due to incompetence or other reasons. The test and reference valves displayed minimal wear on the leaflets. The VIV samples were all well seated. While some abrasions were observed on the valves, the abrasions did not progress to cause tears to the leaflets through the completion of 200 million cycles AWT. No fractures were observed under X-ray in the test and reference valves at the completion of 200 million cycles.

EMBOLISATION

There was no embolisation seen in any of the test articles throughout the testing. The largest migration of any SAPIEN XT within the Magna Ease valve was less than 1.2 millimetres. This occurred in a 25 mm SHV - 26 mm THV VIV combination within the first 20 million cycles and did not progress further.

PART B: IN VITRO VIV DURABILITY STUDY OF SAPIEN XT DEPLOYED INTO EXPLANTED CALCIFIED PERIMOUNT VALVES

All valves met the ISO 5840 minimum performance requirements, which are applicable to replacement valves, for effective orifice area (EOA) and regurgitant fraction at the initiation of the study, at the completion of 20 million cycles, and at the completion of 200 million cycles.

EOA

There was an improvement in EOA with THV deployment. Prior to deployment, the valves had an EOA of $0.44-0.70 \text{ cm}^2$. Post deployment, the EOAs increased to $1.36-2.12 \text{ cm}^2$, and these improved EOAs persisted for the entire study **(Table 3)**.

At the completion of 200 million cycles, the test and reference valves were evaluated against the minimum performance requirement for the EOA as per ISO 5840. The test and reference valves displayed EOA values well above the minimum EOA requirement and met the minimum EOA acceptance criteria (**Table 3**).

REGURGITANT FRACTION

At the completion of the study, the regurgitant fraction for all valves was below the 10% maximum allowable in the ISO for 21 mm and 23 mm valves and also below the 15% maximum allowable in the ISO for 25 mm valves.

AWT DURABILITY TEST

Results show that all valves remained competent through 200 million cycles. Marked improvement in valve performance was

observed when the SAPIEN XT was deployed into the stenotic valve. The test and reference valves displayed minimal wear on the leaflets. No fractures were observed under X-ray in the test and reference valves at the completion of 200 million cycles. **EMBOLISATION**

There was no embolisation seen in any of the test valves throughout the testing. The largest migration of any SAPIEN XT within the explanted PERIMOUNT valve was less than 0.2 millimetres.

Testing for this study was conducted at the research and development laboratories of Edwards Lifesciences, Irvine, CA, USA.

Discussion

Since the first report of a successful VIV case, there has been a rapid increase in the use of THV to treat a failing SHV. There have been at least 16 stented and seven stentless valves manufactured and implanted in the aortic position in the last two decades¹³. Each valve is manufactured in multiple sizes to accommodate variations in patient population. If the label size is known, important dimensions can also be easily obtained¹²⁻¹⁴.

The majority of the experience in VIV has been with two THVs, balloon-expandable SAPIEN/SAPIEN XT and selfexpanding CoreValve⁴⁻¹¹. Recently, other emerging devices have also been used to treat SHV failures in the aortic position, namely the Portico[™] valve (St. Jude Medical, St. Paul, MN, USA) and JenaValve (JenaValve Technology, Munich, Germany)^{17,18}. THVs are designed to enable stability without sutures, hence they rely on relative oversizing to prevent acute or delayed embolisation¹⁹. THVs are manufactured in three to four sizes and are designed to function best when they are expanded fully and retain their end shape, which is mostly circular²⁰.

Despite the many possible combinations, i.e., 16 stented aortic SHVs and four THVs, clinical results have been encouraging⁴⁻¹¹. With increasing usage, however, the VIV treatment does seem to present some unique challenges. One of them is choosing a correct size of THV as undersizing can result in large paravalvular leaks and/or embolisation and oversizing may result in suboptimal function of a THV due to underexpansion²¹. Current recommendations for sizing of THV are an extrapolation of sizing recommendations by THV manufacturers for the native aortic valve^{7,10,13}. Similarly, most of the functional data are available from individual case reports, and case series including VIV registries⁶⁻¹¹. Although satisfactory, the outcomes in small label size valves have been alarming due to higher residual gradients. Mean residual gradients in the global VIV registry have been >20 mmHg in SHVs with ID <20 mm in 58% of patients treated with SAPIEN XT¹¹. Although the causes for this could be multifactorial, it draws attention to the fact that VIV may not offer a good solution in small SHVs with currently available THV and SHV devices.

There is also a paucity of VIV *in vitro* data on issues such as the ideal placement of the THV device, migration/embolisation of the THV device, EOA after VIV (especially in small size SHV) and durability^{15,16}. Hence, we chose to carry out *in vitro* testing with

– The PERIMOUNT pericardial valve has been implanted for more than two decades in large numbers and hence clinicians will be faced with treating these valves with VIV.

- The Magna Ease pericardial valve is currently being implanted due to haemodynamics and it has a large market share. By using a new valve we tried to simulate a worst case scenario after a VIV for each combination as there was absence of calcification or fibrin deposition which would have favoured secure placement. **DEPTH OF IMPLANT**

As the SAPIEN XT is shorter in height compared to other THVs, it is important to ensure correct placement so that it is secure but also prevents SHV leaflet overhang. The sewing ring of the SHV is sutured to the aortic annulus at the time of surgical aortic valve replacement and can provide a reference level for secure anchoring¹⁴. In the Magna Ease and PERIMOUNT the basal band can also provide an additional anchor and visible reference level for placement¹⁴.

In the Magna Ease (supra-annular design), the level of the sewing ring is the same as the level of the basal band (Figure 1B). Thus the SAPIEN XT should be positioned below that level¹⁴. Based on bench testing, we had previously recommended placement of 10-15% of SAPIEN XT below the basal band¹⁴. During *in vitro* testing where attention was also paid to avoid leaflet overhang, we achieved 7-28% of SAPIEN XT lying below the basal band. We saw no THV embolisation. In the PERIMOUNT (Model 2800/2900), the level of the sewing ring is above the basal band (Figure 1A). Hence, we had recommended placement of the SAPIEN XT aligned to the bottom of the basal band¹⁴. This would ensure placement of the SAPIEN XT 10-15% below the sewing ring. *In vitro* testing similar to that of the Magna Ease resulted in placement of the SAPIEN XT 3-16% below the basal band. None resulted in embolisation. There was no SHV leaflet overhang.

The percentage variation was observed due to the relative height difference between the SAPIEN XT and Magna Ease or PERIMOUNT **(Table 1)**, and also due to small variations, which can occur during simulated placement. As one cannot visualise the leaflet edge during a clinical case, it is safer to recommend 10-15% placement of the SAPIEN XT below the basal band for the Magna Ease and 0-5% for the PERIMOUNT as a guide for optimal placement. This is in agreement with the prior work published by our team¹⁴.

EMBOLISATION

Acute or delayed embolisation is another concern if the THV used is smaller than the true ID of the SHV. The test conditions simulated higher than physiological closing pressures and we did not observe significant movement in any of the combinations during these rigorous tests. The only combination where a 1.2 mm downward movement was observed was in one test sample of the Magna Ease 25 with a SAPIEN XT 26 (sample 17202, **Table 2**) where the SAPIEN XT 26 was 24% below the basal band of the Magna Ease 25. We think this is unlikely to happen in a clinical scenario as calcification of SHV leaflets helps to secure the THV⁶⁻¹¹.

HAEMODYNAMICS

Global valve-in-valve registry data have suggested that, for small SHVs, the CoreValve might be better than the SAPIEN XT. Although these are real-world data, the two groups did not appear comparable, as comparison was based on SHV frame ID and not true ID11. True ID is the internal diameter measured after leaflet mounting¹². Derivation of true ID for each SHV make and model has been previously described¹². We have previously demonstrated that SHV design and choice of frame and leaflet materials may cause up to a 2 mm variation in true valve ID¹². Thus, it is possible that valves in the SAPIEN XT group had smaller true ID than those in the CoreValve group despite having similar frame ID. In vitro data have demonstrated optimal EOA in both off-theshelf Magna Ease 21 as well as calcified PERIMOUNT 21 mm when treated with a SAPIEN XT 23. The EOA remained adequate and complied with ISO requirements for the entire duration of the test in all three sizes. The experiment was set up before the new ISO guidelines of 2013 were published. EOAs remained satisfactory for all combinations, even when they were compared with the new ISO 5840-3:2013 guidance. Thus, at 5 lpm and 70 bpm, the EOA for the 21 mm SHV VIV combinations was above 1.2 cm² for all valves (new ISO requirement $\geq 1.05 \text{ cm}^2$), the EOA for the 23 mm SHV VIV combinations was above 1.5 cm² for all valves (new ISO requirement ≥ 1.25 cm²), and the EOA for the 25 mm SHV VIV combinations was above 1.8 cm² for all valves (new ISO requirement $\geq 1.45 \text{ cm}^2$) (Table 2, Table 3).

Azadani et al have carried out an elegant study to evaluate the use of a 23 mm "SAPIEN-like" THV within normal bioprostheses of equivalent or smaller orifice sizes¹⁶. Twelve valves designed to mimic the 23 mm Edwards SAPIEN valve were created using stainless steel stents and trileaflet pericardial valves. A custom-built pulse duplicator was used to measure the haemodynamic performance of these valves within 19, 21 and 23 mm Edwards pericardial bioprostheses. The transvalvular gradient, EOA and regurgitant volume were used to evaluate VIV therapy for each valve size. They observed acceptable VIV haemodynamics only in the 23 mm bioprosthesis after THV implantation, with no significant change in mean pressure gradient (5.93±0.87 to 8.27±1.19 mmHg, p=0.052) and EOA (2.13±0.15 to 1.79±0.15 cm², p=0.053). In 19 and 21 mm valves, they observed severe and moderate stenosis, respectively. The mean pressure gradient increased from 16.18±2.20 mmHg to 45.53±12.54 mmHg (p=0.004) in 19 mm bioprostheses, and from 11.84±1.88 mmHg to 28.18±9.03 mmHg (p=0.004) in 21 mm bioprostheses. Furthermore, the EOA was reduced from 1.28±0.1 to 0.78±0.11 cm² (p<0.001) in 19 mm valves, and from 1.51±0.15 to 1.01±0.19 cm² (p<0.001) in 21 mm bioprostheses. They concluded that the patients with 19 and 21 mm Edwards pericardial bioprostheses may be poor candidates for VIV therapy with the currently available technology. We did not test 19 mm SHV, but haemodynamic results in 21 mm SHV with 23 mm SAPIEN XT were found satisfactory even when used in calcified SHVs with EOA >1.22 cm² and reduction in the mean pressure gradient from 43.2 to 14.5 mmHg **(Table 2, Table 3, Table 4)**. This difference could be due to the refined nature of the SAPIEN XT constructed by a highly complex manufacturing unit versus a hand-made SAPIEN-like device made by Azadani et al. This is supported by observation from a Nordic registry where clinically acceptable gradients were observed in 12 patients with frame ID less than 21 mm¹¹.

Table 4. Mean pressure drops observed with SAPIEN-calcified PERIMOUNT combination.

	Mean pressure drop (mmHg)						
Combination	Before SAPIEN XT	After SAPIEN XT (@ 20 million cycles)	After SAPIEN XT (@ 200 million cycles)				
23S-21P	43.2	14.5	14.7				
23S-23P	52.33	11.6	11.6				
26S-25P	84.4	2.12	1.91				
P: PERIMOUNT; S: SAPIEN XT							

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REGURGITANT FRACTION

Other worries associated with incorrect sizing are PV leak due to undersizing and central leak due to incomplete expansion of a SAPIEN XT. Azadani et al observed an increase in regurgitant volume after VIV for all valve sizes¹⁶. Stent ID and true ID for 21 mm PERIMOUNT and Magna Ease are 20 mm and 19 mm, and for a 23 mm Magna Ease and PERIMOUNT the frame ID and true ID are 22 mm and 21 mm, respectively. We used a 23 mm SAPIEN XT to perform a VIV in these valves. For a 25 mm Magna Ease and PERIMOUNT with frame ID and true ID of 24 mm and 23 mm, we used a 26 mm SAPIEN XT. Hence, with every combination we had incomplete expansion of the SAPIEN XT of 1 to 4 mm. Nevertheless, we observed a very low percentage of leak, well within the limits set by old and new ISO standards.

DURABILITY

Although the attraction of VIV is its less invasive nature, there are concerns about long-term durability. The global VIV registry reported higher residual gradients when VIV was used in the treatment of small SHVs¹¹. It can also be hypothesised that a greater mismatch between true ID and SAPIEN XT size can lead to incomplete expansion and leaflet folding, which may reduce the long-term durability. We found that leaflet durability and function were excellent in all combinations including calcified PERIMOUNT 21 mm and SAPIEN XT 23 mm combinations at the end of 200 million cycles. This is reassuring.

Limitations

The largest percentages of labelled sizes of SHVs implanted are 21, 23 and 25 mm, but 19 mm SHVs are not uncommon and are the most difficult to treat with a VIV due to their very small true ID (17 mm or less). According to the manufacturer's recommendation, the smallest SAPIEN XT, i.e., size 23, can be used in the true ID diameter range of 18 to 22 mm, and hence we did not carry out the testing for the 19 mm surgical valve (true ID of

17 mm). Size 20 mm SAPIEN XT was not available at the time of testing although it is now commercially available. Larger label sizes were not studied as they accept a larger THV. We did not test the SAPIEN XT with SHVs from other manufacturers.

The haemodynamic tests are used to simulate hydrodynamic conditions but do not simulate physiology after human implantation. Tests were carried out at Edwards Lifesciences' facility due to the costs involved in carrying out such a project, namely the cost of heart valves and test equipment.

Conclusions

To conclude, we have demonstrated secure placement, good haemodynamic performance and durability in the six VIV combinations which are commonly seen in clinical practice. Good haemodynamics and durability were also achieved even in SHV size 21 mm with frame ID of 20 mm and true ID of 19 mm when using a 23 mm SAPIEN XT transcatheter heart valve.

Impact on daily practice

Valve in valve is fast becoming a preferred modality of treatment for a degenerated surgical bioprosthesis. With a wide choice of multiple TAVI devices, it is important to use the right device, especially in small size bioprostheses. Our study provides robust early- and midterm outcomes as per ISO guidelines and will give confidence to the users to implant the SAPIEN XT in daily practice. Further, they can be assured of the durability of the newly implanted SAPIEN XT.

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Conflict of interest statement

V. Bapat is a consultant for Edwards Lifesciences, Medtronic, Boston Scientific and St. Jude Medical. D. Chambers has no conflicts of interest to declare.

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