

# Endovascular aortic repair in patients with challenging anatomies: the EXTREME study



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## KEYWORDS

- abdominal aorta aneurysm
- abdominal aortic aneurysm stent/prosthesis
- clinical trials

## Abstract

**Aims:** The aim of this study was to report the 30-day technical and clinical success with endovascular repair using the ultra-low-profile Ovation stent graft in patients judged to be outside the instructions for use (IFU) for conventional endografts, while amenable to treatment within the IFU for Ovation.

**Methods and results:** One hundred and twenty-two patients (78.65±7.67 years; 111 male) were enrolled. Patients were evaluated as being outside the IFU for standard endografts because of the absence of a suitable proximal aortic neck in 109 cases (89.3%), of inadequate access vessels in 13 (10.7%), or both in 111 (90.9%). Mean aneurysm (abdominal aortic aneurysm [AAA]) diameter was 52.96±10.1 mm; mean aortic neck length was 7.75±6.05 mm. Technical success (98.4%) was achieved in all but two patients due to a type Ia endoleak. At completion angiography, 15 (12.3%) patients presented a type II endoleak. All patients underwent 30-day follow-up. Primary clinical success at one month was 96.8%, assisted clinical success 98.4%. There were no type I endoleaks, while 12 (9.8%) type II endoleaks were still evident, in the absence of sac expansions. Two patients (1.6%) presented an asymptomatic limb occlusion.

**Conclusions:** Our experience suggests that, in a selected population of patients with challenging anatomy outside the IFU for conventional endografts, endovascular aneurysm repair (EVAR) using the Ovation stent graft can be performed safely with satisfactory immediate outcomes.

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## Abbreviations

<b>AAA</b>	abdominal aortic aneurysm
<b>CIA</b>	common iliac artery
<b>CTA</b>	computed tomography angiography
<b>EIA</b>	external iliac artery
<b>EVAR</b>	endovascular aneurysm repair
<b>IFU</b>	instructions for use
<b>IR</b>	inferior renal artery
<b>ITR</b>	iliac tortuosity ratio

## Introduction

Endovascular aneurysm repair (EVAR) has become the standard of care for abdominal aortic aneurysm (AAA) in patients presenting with standard anatomies<sup>1,2</sup>. Nowadays, performing EVAR outside the devices' specific instructions for use (IFU), particularly in the presence of a so-called "challenging neck"<sup>3</sup>, yields a not negligible rate of immediate complications and reinterventions<sup>4,5</sup>. Of note, any differences in outcome between patients presenting with or without a challenging anatomy were lost during follow-up<sup>6</sup>. Consequently, several different technical solutions, such as parallel grafts, fenestrated or branched devices, have been developed as an alternative to standard EVAR grafts in patients with a "challenging neck". However, all those solutions present a relevant risk of reintervention due to branch-related complications<sup>7</sup>.

In recent years, a new sealing concept based on polymer has become available for the treatment of AAA, and two devices have become available, the Ovation<sup>®</sup> stent graft<sup>8,9</sup>, and Nellix<sup>®10</sup> (both from Endologix Inc., Irvine, CA, USA).

The Ovation endograft in particular represents a new technical step in EVAR<sup>8,9</sup>, separating fixation from sealing. It seems to increase the range of AAAs suitable for standard EVAR procedures, as reported in several, although limited, series<sup>11-13</sup> (**Supplementary Appendix 1**).

To confirm the results in a larger, multicentre, and coordinated series, a new physician-initiated study has been designed—Expanding Indications for Treatment with Standard EVAR in Patients with Challenging Anatomies, a Multi-Centric Prospective Evaluation (EXTREME) – aiming to report technical and clinical success of EVAR using the Ovation platform in patients judged to be outside the IFU for conventional bifurcated endografts, while amenable to treatment inside the IFU for the Ovation stent graft. In the present paper, 30-day technical success and clinical success are reported<sup>14</sup>.

## Methods and material

From March 2017 to March 2018 investigators enrolled all consecutive patients matching the inclusion criteria for the study. Clinical and anatomical data are collected in an anonymised prospectively compiled database including baseline, hospital discharge, 1-month, and 12-month evaluations.

The inclusion criterion for the study was AAA requiring elective treatment in patients judged to be outside of the IFU for commercially available bifurcated endografts, while inside the IFU for the Ovation.

According to the manufacturer's IFU, anatomical requirements, evaluated on preoperative computed tomography angiography (CTA), were: proximal aortic landing zone presenting an inner wall diameter of no less than 16 mm and no greater than 30 mm at 13 mm below the inferior renal artery (IR), and an aortic angle of  $\leq 60^\circ$  if the proximal neck is  $\geq 10$  mm and  $\leq 45^\circ$  if the proximal neck is  $< 10$  mm; presence of an iliac landing zone at least 10 mm in length, and with an inner wall diameter of no less than 8 mm and no greater than 25 mm; iliac and femoral access compatible with vascular access techniques, devices, and accessories.

This study complied with the principles of the Declaration of Helsinki and, when requested, the data collection and acquisition were approved by the local ethics committee and respective institutional review boards of each site. Informed consent from the patients was obtained for the procedures but was not required for the study.

Endovascular procedures were performed by vascular surgeons in the operating theatre equipped with a portable fluoroscopy unit (**Supplementary Appendix 2**).

Albeit local anaesthesia was generally preferred for frail patients<sup>15</sup>, the centres involved were left free to choose between general and local anaesthesia.

All patients were monitored postoperatively with clinical evaluation and duplex ultrasound examination before discharge and at one month. CTA was performed per protocol in all enrolled patients one month after the index EVAR procedure.

In all cases, the landing distance, defined as the distance between the lowest renal artery ostium and the endograft proximal markers, was noted. Complications that occurred during and after the EVAR procedure were classified as per the reporting standards for endovascular aortic aneurysm repair<sup>16</sup>.

Clinical endpoints were freedom from AAA-related mortality, procedure-related serious and non-serious adverse events, AAA enlargement ( $\geq 5$  mm), and AAA rupture. Technical endpoints were procedural success (complete delivery and deployment of one aortic body and two iliac limbs), access-related vascular complications, freedom from type I and III endoleaks, freedom from graft migration ( $\geq 5$  mm), conversion to open repair, and all AAA-related secondary interventions.

Clinical success is defined as successful deployment of the endovascular device at the intended location without death as a result of aneurysm-related treatment, type I or III endoleak, graft infection or thrombosis, aneurysm expansion (diameter  $> 5$  mm, or volume  $> 5\%$ ), aneurysm rupture, or conversion to open repair.

An AAA-related adverse event is defined as a composite of the following: direct (type I or III) or undetermined type endoleaks, aneurysm sac growth, migration, device integrity failure, AAA-related death, late post-implantation AAA rupture or any AAA-related secondary intervention.

Secondary interventions are considered if performed to resolve or prevent a possible complication. These include endovascular procedures (proximal cuff and stent implant, coil or glue embolisation, distal extension implant, catheter-based thrombolysis, iliac

angioplasty) as well as surgical procedures (balloon thrombectomy, femoro-femoral crossover, conversion to open repair, open or laparoscopic ligation of collaterals).

To avoid any potential interpretation bias, preoperative, and postoperative CTA data were collected and sent for blind reading by a centralised core laboratory (Vascular and Endovascular Surgery, “Sapienza” University of Rome) using dedicated software with multiplanar and volume reconstructions (OsiriX MD; Pixmeo SARL, Bernex, Switzerland) on a Mac OS computer (Apple Inc., Cupertino, CA, USA)<sup>17</sup>. AAA diameter, infrarenal diameter, IR+13 diameter, aortic neck length and shape, aortic neck thrombosis and calcification,  $\alpha$  and  $\beta$  angles, aortic bifurcation diameter, area, thrombosis, and calcification were noted and evaluated as potentially influencing the outcome. Iliac artery anatomical features are common iliac artery (CIA) and external iliac artery (EIA) diameters, iliac access thrombosis/calcification, and iliac tortuosity ratio (ITR)<sup>18</sup>. For both the aortic neck and the iliac access vessels, calcification and thrombosis were considered as “severe”, and potentially influencing results, when accounting for >50% of circumferential involvement in an axial projection.

All CTAs were independently evaluated by two vascular surgeons (P. Sirignano, S. Cuozzo). Disagreements were discussed and resolved by consensus.

### STATISTICAL ANALYSIS

Continuous data are reported as mean, median, standard deviation and range, for continuous variables. Frequency and percentages are reported for categorical variables.

### Results

One hundred and thirty-four patients were screened; 122 (mean age, 78.65±7.67 years; 111 male) were treated with EVAR using the Ovation stent graft system at 16 European vascular centres from a total of 527 EVAR procedures performed (median 32.9 patients/year per centre) during the entire study period. Demographic data and risk factors for all enrolled patients are described in **Supplementary Table 1**. Patients who were screened but not enrolled were treated by different surgical or endovascular (chimney EVAR, or fenestrated endograft) procedures.

Detailed anatomical features of all patients enrolled in the present series are reported in **Table 1** and **Supplementary Appendix 3**.

All procedures in this series were performed by highly skilled vascular surgeons with an experience of at least 30 Ovation stent-graft implantations. Percutaneous access was used in 101 (82.8%) patients, and local anaesthesia in 109 (89.3%). Mean endograft oversizing was 19.59±5.68% (range 8.6-36%). Mean operative time was 64±26 minutes and contrast amount 76±18 ml. No patient required postoperative intensive care unit stay; mean postoperative length of stay was 2.27±1.43 days (range 1-10).

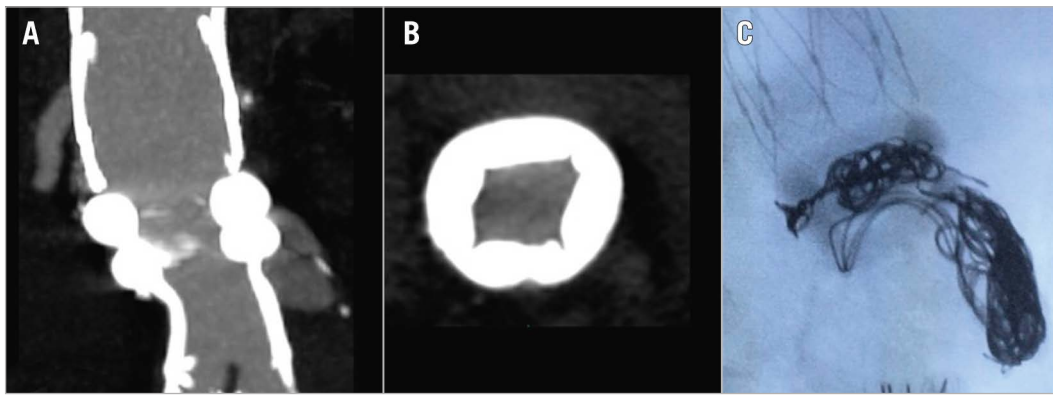
Technical success was achieved in all but two patients (1.6%) due to a type Ia endoleak, and in one case (0.8%) a partial polymer leak was noted during ring inflation without evidence of endoleak. At completion angiography, 15 (12.3%) patients presented a type II

**Table 1. Preoperative anatomical features of abdominal aortic aneurysms treated in the present series.**

	Total patients 122
AAA max diameter, mean±SD (range)	52.96±10.1 mm (33-102)
IR diameter, mean±SD (range)	21.96±3.46 mm (15.9-32)
IR+13 diameter, mean±SD (range)	24.24±3.31 mm (18-30)
IR+16 diameter, mean±SD (range)	24.67±4.72 mm (17-33)
Aortic neck length, mean±SD (range)	7.75±6.05 mm (1-29.5)
Aortic neck length <5 mm (n; %)	35; 28.7
Aortic neck length 5-10 mm (n; %)	51; 41.8
Aortic neck length >10 mm (n; %)	36; 29.5
Cylindrical aortic neck shape (n; %)	41; 33.60
Aortic neck thrombosis/calcification (n; %)	73; 59.83
$\alpha$ angle, mean±SD (range)	17.73±11.58° (2-63)
$\beta$ angle, mean±SD (range)	21.39±18.99° (2-60)
Aortic bifurcation diameter, mean±SD (range)	24.14±8.62 mm (8.1-57.6)
Aortic bifurcation area, mean±SD (range)	5.69±4.54 mm <sup>2</sup> (1.1-25.3)
Aortic bifurcation area thrombosis/calcification (n; %)	64; 52.45
Right CIA diameter, mean±SD (range)	14.23±9.77 mm (6-90)
Right CIA diameter >20 mm (n; %)	9; 7.37
Right CIA diameter 10-20 mm (n; %)	90; 73.77
Right CIA diameter <10 mm (n; %)	23; 18.85
Left CIA diameter, mean±SD (range)	13.61±8.73 mm (4-77)
Left CIA diameter >20 mm (n; %)	20; 16.39
Left CIA diameter 10-20 mm (n; %)	86; 70.49
Left CIA diameter <10 mm (n; %)	29; 23.77
Right EIA diameter, mean±SD (range)	7.6±2.07 mm (4.1-7.7)
Right EIA diameter <10 mm (n; %)	106; 86.88
Right EIA diameter <7 mm (n; %)	32; 26.22
Left EIA diameter, mean±SD (range)	7.33±1.59 mm (2-11.1)
Left EIA diameter <10 mm (n; %)	114; 93.44
Left EIA diameter <7 mm (n; %)	42; 34.42
Iliac access thrombosis/calcification (n; %)	52; 42.66
Right iliac access ITR, mean±SD (range)	0.76±0.09 (0.5-0.96)
Left iliac access ITR, mean±SD (range)	0.8±0.1 (0.5-0.98)
AAA: abdominal aortic aneurysm; CIA: common iliac artery; EIA: external iliac artery; IR: infrarenal; ITR: iliac tortuosity ratio	

endoleak. The patient with a polymer leak suffered a lumbar skin necrosis treated by vacuum-assisted therapy with complete healing at the one-month follow-up visit.

Regarding the two reported type Ia endoleaks, one case was secondary to infolding of the first ring (**Figure 1A, Figure 1B**) as a result of an excessive oversizing of the endograft (>30%), while in the other case the endoleak was due to an intraprocedural error, i.e., the endograft was released below the preoperatively evaluated sealing zone (at IR+18, instead of IR+13). Both type Ia endoleaks were successfully treated by endovascular coil embolisation during the same hospitalisation (**Figure 1C**) with complete aneurysm exclusion and absence of further complications.



**Figure 1.** Type Ia endoleaks following EVAR procedure. A) Multiplanar reconstruction of the postoperative CTA showing a type Ia endoleak. B) Axial postoperative CTA image showing infolding of the proximal sealing ring due to excessive oversizing. C) Intraoperative lateral image with coils placed between the two rings, exactly where the infolding was responsible for the leakage.

All enrolled patients underwent a scheduled 30-day follow-up visit and CTA. Primary clinical success at one month was 96.8% (defined as the absence of aneurysm-related death, type I or III endoleak, graft infection or thrombosis, aneurysm expansion >5 mm, aneurysm rupture, or conversion to open repair). Assisted clinical success at one month was 98.4% (Table 2). Mean landing distance at postoperative CTA was  $0.92 \pm 0.18$  mm (range 0-5 mm).

**Table 2. Primary and assisted clinical success at 1 month in the present series.**

	Total patients 122
Primary clinical success (n; %)	118; 96.8%
Aneurysm-related death	0
Type I or III endoleak*	2; 1.6%
Aneurysm expansion*	0
Graft infection	0
Graft thrombosis*	2; 1.6%
Conversion to open repair	0
Assisted primary clinical success (n; %)	120; 98.4%
Aneurysm-related death	0
Type I or III endoleak*	0
Aneurysm expansion*	0
Graft infection	0
Graft thrombosis*	2**; 1.6%
Conversion to open repair	0

\* assessed by CT and/or ultrasound follow-up. \*\* asymptomatic iliac limb occlusion, medically managed.

There were no type I or III endoleaks, although 12 (9.8%) type II endoleaks were still evident, in the absence of sac expansions. Two patients (1.6%) presented an asymptomatic iliac limb occlusion, medically managed. No further complications, reinterventions or deaths were recorded at that time.

## Discussion

Anatomic constraints represent the main exclusion criteria for EVAR in a real-world setting. However, with increasing operator experience, a tendency to push limits has become apparent and there are now data to indicate that EVAR may be safe even if the AAA configuration does not entirely fall within the pre-specified requirements of each endograft. Several reports suggesting a similar technical and clinical success rate between patients treated within or outside the endograft's IFU have been published<sup>3,6,19,20</sup>. On the other hand, other authors have reported significantly inferior outcomes among patients treated outside the IFU. Sac enlargement and type Ia endoleak rates were both significantly related to adherence to device guidelines<sup>21-24</sup>. Indeed, patients with hostile anatomy were found to present a fourfold increased risk of developing type I endoleak and a ninefold increased risk of aneurysm-related mortality<sup>25</sup>.

Historically, irrespective of the type of endograft, EVAR eligibility has been considered for aortic neck length >15 mm, angulation <60° and diameter 18-30 mm, and a distal landing zone <20 mm in diameter with an access vessel diameter >7 mm. During the evolution from the first to the fourth generation of endografts, significant refinements have been introduced in order to accommodate a broader range of anatomies, for example a neck length of 10 mm, a juxtarenal angulation up to 90°, and adaptability to navigate vessels as narrow as 4.7 mm. Considering these parameters, suitability for EVAR has reportedly been extremely low<sup>26</sup>. A meta-analysis published by Ulug et al in 2017 evaluated the morphological eligibility for EVAR in 1,507 men and 400 women. The overall pooled proportion of eligible women was 34%, which was lower than that in men, estimated at 54%<sup>27</sup>. Sweet et al, examining >1,000 patients using the traditional criteria to define suitable anatomy, reported low rates of both men (32%) and women (12%) meeting all neck criteria and having adequate iliac lumen diameters<sup>28</sup>.

As mentioned above, the Ovation stent graft presents a unique design and concept, uncoupling the sealing and fixation modes of the device, and a very low profile<sup>29</sup>. Those differences increased

eligibility rates remarkably compared with other commercially available endografts, as demonstrated by Kontopodis et al. In their retrospective analysis of 158 consecutive AAA patients treated with EVAR or open surgical repair, eligibility rates were significantly higher for the Ovation (72%) compared to the other endografts<sup>13</sup>. A high rate of eligibility was confirmed by data presented in our series: only 12 out of 134 patients evaluated were judged not to fit the Ovation IFU and were treated with different surgical or endovascular procedures. In the 122 treated patients, technical success was achieved in all but two patients. Assisted clinical success at one month was 98.4% in patients who were judged to be outside the IFU for standard endografts because of the absence of a suitable proximal aortic neck (89.3%), inadequate access vessels (10.7%), or both (90.9%). Our results in such a highly selected anatomically challenging population were consistent with those reported in a pivotal study<sup>30</sup>, confirming the initial hypothesis of the study. In the present series, two patients presented a type Ia endoleak (1.6%), both consequent to preprocedural or intra-procedural mistakes, while no type Ia endoleak but four undefined endoleaks (2.48%) were reported by Mehta et al in the pivotal study. The rates of iliac occlusion were similar (1.6% in the present study and 0.6% in the pivotal study). Notably, type II endoleak incidence was slightly lower in our series, i.e., 9.8% vs 25.46%<sup>30</sup>.

Regarding the two reported limb occlusions, core lab analysis was unable to identify a possible cause: limbs were implanted in relatively straight anatomies, in the absence of severe stenosis. Speculatively, both patients presented a chronic peripheral arterial disease that could have favoured the occlusions.

Moreover, the polymer-filled sealing rings (an exclusive characteristic of the Ovation stent graft) conform to patients' proximal aortic neck anatomy, creating an uninterrupted concentric seal reminiscent of an O-ring or the gasket-like seals that have long been considered the standard in other sealing applications. Providing a simple, precise and reliable seal in a variety of applications and functions by introducing a calculated mechanical stress between the O-ring and the surface, the ring is in contact with a solution to prevent fluid or air from passing between two surfaces. Being cast *in situ* to form a custom-modelled O-ring seal at the margin of the AAA, the polymer guarantees high seal conformability on irregular surfaces, such as in the presence of calcium and thrombus<sup>28</sup>. This feature played a crucial role in treating AAA patients presenting an extremely short or even absent proximal aortic neck.

A previously published paper demonstrated that the filled polymer does not apply chronic outward force on the aorta, which is likely with other endografts that employ oversized, self-expanding stents to achieve sealing in the proximal aortic neck<sup>31</sup>, while the use of self-expanding stent grafts has been clearly related to neck progression because those grafts continue to expand until the nominal diameter is reached<sup>32</sup>, unless tissue resistance limits expansion<sup>33</sup>.

It is well known that when aortic neck dilation occurs it affects EVAR procedural outcomes in the midterm and long term<sup>34</sup>. Conversely, Ovation stent graft implantation has not been associated with this phenomenon and should be considered protective in

midterm and long-term follow-up, as reported by de Donato et al<sup>31</sup>. This finding needs to be confirmed in our series of very selected, extremely challenging patients once 12-month CTA becomes available.

## Limitations

The present study has several limitations. Firstly, it is a non-randomised study with a relatively small number of enrolled subjects. Furthermore, the procedures included in this cohort were performed by operators in an advanced phase of their learning curve, which could partially explain the small number of reinterventions in such a complex cohort of patients.

Despite the early results presented in this study demonstrating the safety and technical efficacy of the Ovation endografts implanted in patients not amenable to be treated with other standard devices within the IFU, we should admit that it is well known that the great majority of adverse events after EVAR occur in the midterm and long-term follow-up<sup>35</sup>. With the aim of confirming our initial findings, follow-up data collection and analysis are still ongoing.

## Conclusions

Preliminary available data from this real-world multicentric study seem to confirm the hypothesis that AAA repair by EVAR with Ovation stent-graft implantation can be performed safely, even in extremely complex anatomies evaluated as being unfit for conventional stent grafts. Preliminary one-month data are promising, showing only a 1.6% rate of high flow proximal endoleak requiring endovascular reintervention and a very high assisted clinical success rate at one month. However, a longer follow-up is needed to confirm these initial findings.

### Impact on daily practice

The present paper concerns a multicentre prospective non-randomised study. Our key finding was that endovascular treatment of abdominal aortic aneurysms in 122 patients judged to be outside of the instructions for use (IFU) for conventional endografts, and amenable to treatment within the IFU for the Ovation stent graft resulted in 96.8% primary clinical success, and 98.4% assisted clinical success at one month. Data suggest that AAA repair by EVAR with Ovation stent-graft implantation can be performed safely even in extremely complex anatomies evaluated unfit for conventional stent grafts.

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## Conflict of interest statement

The authors/study collaborators have no conflicts of interest to declare.

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## Supplementary data

**Supplementary Appendix 1.** Ovation stent graft characteristics.

**Supplementary Appendix 2.** Description of ovation stent graft.

**Supplementary Appendix 3.** Anatomical characteristics of patients included in present analysis.

**Supplementary Table 1.** Patient demographics, characteristics, and risk factors in the present series.

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## **Supplementary data**

### **Supplementary Appendix 1. Ovation stent graft characteristics**

Suprarenal stent and anchors are responsible for graft fixation, while sealing is provided by inflatable rings filled with a low-viscosity, non-embolic, radiopaque fill polymer. The presence of the polymer-filled network also allows the graft to conform to the patient's aortic neck, providing a precise and reliable sealing in a great variety of anatomies. Different from common stent graft platforms, separation between fixation and sealing ensures that in the Ovation stent graft and fabric do not compete for the same space within the shaft and an ultra-low-profile delivery system can be used, allowing the treatment of patients presenting with a wide range of iliac access.

### **Supplementary Appendix 2. Description of Ovation stent graft implantation technique**

Subsequent to femoral access, the tri-modular stent graft was delivered and deployed in three stages: unsheathing the main body, deploying the suprarenal bare metal stent, and injecting the amount of polymer needed to expand the stent-graft main body rings that subsequently conform to the aortic neck (so-called "customised proximal sealing"). The iliac rings along the main body provide support for the ipsilateral and contralateral iliac extensions. In accordance with the IFU, the extra-support guidewire was partially retracted during polymer delivery, in order to allow the stent graft to conform to the native aortic anatomy. The contralateral gate was usually engaged during polymerisation time. The iliac limbs were subsequently deployed. In all cases, a kissing balloon angioplasty to achieve optimal sealing between the main body and iliac limbs was carried out, followed by ballooning of the iliac sealing zones. Post-dilatation of the polymer rings was not routinely performed except in case of a type Ia endoleak seen at completion angiography and within 40 minutes from polymer injection. Whenever possible, oversizing was chosen complying with the manufacturer's IFU. Surgical cutdown to the groin and a percutaneous approach were both performed. In case of percutaneous access, haemostasis was achieved using single or double Perclose-ProGlide® (Abbott Vascular, Santa Clara, CA, USA) implantation.

### **Supplementary Appendix 3. Anatomical characteristics of patients included in present analysis**



Mean AAA diameter was  $52.96 \pm 10.1$  mm (range 33-102), mean IR diameter  $21.96 \pm 3.46$  mm (15.9-32), mean IR+13 was  $24.24 \pm 3.31$  mm (18-30), and mean IR+16 was  $24.67 \pm 4.72$  mm (17-33). Mean aortic neck length was  $7.75 \pm 6.05$  mm (1-29.5); in particular, aortic neck length was <10 mm in 86 cases (70.4%), between 5 and 10 mm in 51 (41.8%), and <5 mm in 35 (28.7%). Forty-one patients (33.6%) presented a cylindrical aortic neck, while in 73 (59.83%) treated cases severe calcification and/or thrombosis of the proximal neck was reported.

Mean aortic bifurcation diameter and area were  $24.14 \pm 8.62$  mm (8.1-57.6) and  $5.69 \pm 4.54$  mm<sup>2</sup> (1.1-25.3), respectively. Mean CIA diameters were  $14.23 \pm 9.77$  mm (6-90) and  $13.61 \pm 8.73$  mm (4-77), respectively, on the right and left side; EIA diameters were  $7.8 \pm 2.07$  mm (4.1-7.7) and  $7.33 \pm 1.59$  mm (2-11.1).

**Supplementary Table 1. Patient demographics, characteristics and risk factors in the present series.**

	<b>Total patients 122</b>
Age (mean±SD)	78.65±7.67
Male sex (n; %)	111; 90.98
Hypertension (n; %)	106; 86.88
Dyslipidaemia (n; %)	85; 69.67
Diabetes (n; %)	78; 63.93
CAD (n; %)	69; 56.55
Smoking (n; %)	83; 68.03
COPD (n; %)	67; 54.91
CRI (n; %)	45; 36.88
PAOD (n; %)	37; 30.32
ASA III/IV (n; %)	32; 26.22

CAD: coronary artery disease; COPD: chronic obstructive pulmonary disease; CRI: chronic renal insufficiency; PAOD: peripheral arterial obstructive disease