Assessment of arterial stiffness to predict blood pressure response to renal sympathetic denervation

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KEYWORDS

•MRI

- renal sympathetic denervation
- resistant hypertension
- •uncontrolled hypertension

Abstract

Background: Recent trials support the efficacy of renal sympathetic denervation (RDN) to reduce blood pressure (BP). Nevertheless, about one third of patients are considered non-responders to RDN. Previous retrospective analyses suggest arterial stiffness could predict BP response to RDN.

Aims: We prospectively assessed the potential of invasive pulse wave velocity (iPWV) to predict BP response to RDN. Additionally, we aimed to establish non-invasive models based on arterial stiffness to predict BP response to RDN.

Methods: iPWV magnetic resonance imaging-based markers of arterial stiffness and the carotid-femoral pulse wave velocity were recorded prior to RDN in patients with treatment resistant hypertension. Changes in daytime BP after 3 months were analysed according to the prespecified iPWV cut-off (14.4 m/s). Regression analyses were used to establish models for non-invasive prediction of BP response. Results were compared to iPWV as reference and were then validated in an external patient cohort.

Results: Eighty patients underwent stiffness assessment before RDN. After 3 months, systolic 24h and daytime BP were reduced by 13.6 \pm 9.8 mmHg and 14.7 \pm 10.6 mmHg in patients with low iPWV, versus 6.2 \pm 13.3 mmHg and 6.3 \pm 12.8 mmHg in those with high iPWV (p<0.001 for both). Upon regression analysis, logarithmic ascending aortic distensibility and systolic baseline BP independently predicted BP change at follow-up. Both were confirmed in the validation cohort.

Conclusions: iPWV is an independent predictor for BP response after RDN. In addition, BP change prediction following RDN using non-invasive measures is feasible. This could facilitate patient selection for RDN treatment.

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Abbreviations

mTAC total arterial compliance (magnetic resonance imaging)

Introduction

Effective treatment of hypertension, the major preventable cause of mortality worldwide, remains a very significant global public health concern¹. Depending on the definition used, 5-30% of patients in whom blood pressure (BP) control, by means of lifestyle modification and medical treatment, fails, suffer from resistant hypertension¹. In the past decade, an interventional treatment approach of catheter-based renal sympathetic denervation (RDN) has emerged as a potential alternative for these patients. Recent randomised trial results support the efficacy of this treatment in reducing BP in comparison to sham treatment²⁻⁵. Nevertheless, all these trials uniformly report that about one third of patients do not experience relevant BP reduction following the intervention. To enhance the efficacy of RDN, reducing the variability of BP response to the intervention has been suggested to be of utmost importance⁶. Therefore, early identification of patients who benefit from RDN (responders) and those who are unlikely to respond (non-responders) seems crucial.

It has been suggested that an assessment of arterial stiffness could be useful in predicting response to RDN7 . In previous studies from our group, elevated invasive pulse wave velocity (iPWV) as a surrogate for vascular stiffness has been identified as a predictor of a poor BP response following $RDN⁸⁻¹⁰$. As estimation of iPWV requires catheterisation, non-invasive measures to estimate the success of RDN are desirable. As such, magnetic resonance imaging (MRI)-derived markers of arterial stiffening, such as ascending aortic distensibility (mAAD) and total arterial compliance (mTAC), seem to have some predictive value, but further research is necessary¹¹. Similarly, the carotid-femoral pulse wave velocity (cPWV), as assessed using bedside tools $12,13$, may be an easy and cost-effective method to estimate arterial stiffness, but its value in prediction of BP response to RDN is not well described.

To improve patient selection for RDN, we conducted a trial to prospectively confirm iPWV as a predictor of RDN response and to investigate the potential of different non-invasive estimates for arterial stiffness to predict a BP response to RDN.

Methods

TRIAL DESIGN

We conducted a prospective single-centre clinical trial in patients undergoing intravascular ultrasound RDN to:

- 1. confirm the value of a predefined invasive pulse wave velocity (iPWV) as a predictor of BP response after RDN (primary outcome),
- 2. develop prediction models for (a) linear and (b) binary (≥5 mmHg) 24h BP response after RDN, using non-invasive markers of arterial stiffness and clinical characteristics and to compare them with iPWV (exploratory outcome),
- 3. validate these models and findings using an external cohort of patients (validation outcome). Validation was not predefined but was implemented retrospectively.

The study was approved by the local ethics committee and was performed in accordance with the Declaration of Helsinki. All participants provided written informed consent. The trial is registered at ClinicalTrials.gov: NCT02772939.

STUDY PARTICIPANTS

Patients were screened if diagnosed with resistant hypertension (office BP >160 mmHg systolic or >90 mmHg diastolic, despite treatment with 3 or more different classes of antihypertensive drugs on at least 50% of maximum dosage for hypertension, including at least one diuretic, unless intolerant to diuretics). Antihypertensive medication had to be stable for at least 4 weeks. Patients then underwent ambulatory blood pressure measurement (ABPM) to assess baseline ABPM values. Inclusion criteria were resistant hypertension with systolic daytime BP >135 mmHg on ABPM. Exclusion criteria were <18 or >75 years old, pregnancy, life expectancy <6 months, evidence of untreated secondary hypertension, known renal artery stenosis or anatomy unsuitable for interventional RDN and any main renal artery diameter <4.0 mm. Further details on study participants, BP measurement and exclusion of secondary hypertension can be found in **Supplementary Table 1**.

INVASIVE MEASUREMENT OF ARTERIAL STIFFNESS

iPWV was determined by invasive measurements prior to RDN and sedation. A 7 Fr sheath was placed in the right femoral artery and a 4 Fr pigtail catheter (Cordis) in the ascending aorta. Simultaneous pressure curves were recorded through the pigtail and the sheath's side-port. The foot-to-foot method was used to determine iPWV, as previously described¹⁰.

MAGNETIC RESONANCE IMAGING-BASED ASSESSMENT OF **STIFFNESS**

All patients underwent MRI before RDN to assess mTAC, mAAD and MRI-based pulse wave velocity (mPWV). Details of the MRI protocol as well as estimation of the different markers of vascular stiffness can be found in the **Supplementary Appendix 1**.

CAROTID-FEMORAL PULSE WAVE VELOCITY

Non-invasive values for cPWV were measured with a dedicated piezoelectric device and software (Complior Analyse; Alam Medical)13. Measurements were taken in a supine position after at least 5 minutes of rest in a quiet environment and before RDN. Two full measurements, consisting of 5-10 heart cycles, were averaged.

RDN PROCEDURE

Endovascular ultrasound RDN was performed using the Paradise catheter (ReCor Medical), a balloon-cooled device that creates a fully circumferential thermal ablation pattern using acoustic energy. Details of the procedure have been published previously2,4,14. All procedures were performed by experienced interventional cardiologists with experience in ultrasound RDN.

DEFINITIONS

Binary blood pressure response (BBPR) was defined as reduction of ≥5 mmHg in 24h systolic BP on ABPM at 3 months, which was deemed as clinically relevant in a previous consensus statement on RDN⁷.

An optimal sensitivity threshold (OST) was defined as the value with a 90% sensitivity to detect BBPR after 3 months in the study cohort.

FOLLOW-UP AND OUTCOMES

At 3 months, ABPM was repeated to assess the primary endpoint. Medication changes and adherence were assessed at 1 and 3 months through structured interviews with patients.

The trial was designed to address 2 outcomes: the primary endpoint was the change in systolic daytime BP on ABPM at 3 months between patients above and below the predefined pulse wave velocity cut-off of 14.4 m/s, derived from prior retrospective analyses¹⁰. Key secondary outcomes were the areas under the receiver operator characteristics (ROC) curves and linear regression coefficients for non-invasive models to predict BP response in comparison to iPWV. We: 1) identified independent predictors and multivariable models for linear 24h BP change, 2) calculated ROC curves and OSTs for each model, 3) compared ROC curves and linear regression coefficients, 4) validated the OSTs in an external validation cohort **(Central illustration)**.

STATISTICAL ANALYSIS

Linear and logistic regression, ROC curves and areas under the curves (AUC) were calculated for the prediction of linear BP response and BBPR to RDN. Details on the uni- and multivariable regression analyses as well as on sample size calculation can be found in the **Supplementary Appendix 1**.

G-Power 3.1.9.2 was used for power calculation (University of Düsseldorf, Germany)¹⁵. All other statistical analyses were calculated with SPSS 24.0.0.0 and 28.0.0.0 (IBM) and MedCalc 16.4.3 (MedCalc Software).

Results

Between June 2015 and May 2020, 80 patients were enrolled **(Figure 1)**. All patients underwent bilateral RDN. One patient was lost to follow-up. Survival status for this patient was confirmed by contacting the treating general practitioner and the subject was excluded from further analysis. In total, 79 patients were available for final analyses.

BASELINE CHARACTERISTICS AND BP OUTCOME

Clinical baseline characteristics, blood pressure and medication are shown in **Table 1**. Details of medication adherence can be found in

Euro**Intervention**

CENTRAL **ILLUSTRATION Prediction of RDN response in treatment resistant hypertension.**

**p<0.05; n.s.: not significant; ABPM: ambulatory blood pressure monitoring; BP: blood pressure; iPWV: invasive pulse wave velocity; MRI: magnetic resonance imaging; OST: optimal sensitivity threshold; RDN: renal denervation*

Figure 1. *Study flow. MRI: magnetic resonance imaging; PWV: pulse wave velocity*

Supplementary Appendix 2. At 3 months, 24h systolic and diastolic BP values were reduced by $10.0/6.7 \pm 12.2/8.0$. Corresponding daytime BP values were reduced by $10.5/7.1 \pm 12.4/8.0$ mmHg (p<0.001) for all). Forty-seven patients (59%) were classified as having a BBPR.

CONFIRMATION OF iPWV AS A PREDICTOR FOR BP REDUCTION

In comparing patients with low iPWV $(\leq 14.4 \text{ m/s})$ and patients with high baseline iPWV, baseline characteristics were balanced between the groups, except for age, which was higher in the high iPWV group **(Supplementary Table 1)**. Patients with low iPWV had a significantly greater reduction of 24h and daytime systolic and diastolic BP (p<0.01 for all) **(Figure 2)**.

In a linear regression model, iPWV was confirmed as an independent predictor for daytime and 24h BP reduction at follow-up (Beta=0.242 and 0.232) **(Supplementary Table 2)**.

iPWV was poorly correlated with 24h systolic BP change after 3 months in a linear or logarithmic fashion (r^2 =0.055 and 0.076, p=0.04 and 0.01, respectively). AUC for prediction of BBPR was 0.695. BBPR frequencies were 44% in patients with high iPWV and 75% in patients with low iPWV (p=0.001). Upon logistic regression, iPWV was an independent predictor of BBPR (p=0.019).

Figure 2. *Primary outcome: blood pressure changes in patients with low (<14.4 m/s) vs high (≥14.4 m/s) invasive pulse wave velocity. Error bars indicate 95% confidence intervals. iPWV: invasive pulse wave velocity*

Table 1. Baseline characteristics and medication (n=80).

EXPLORATORY NON-INVASIVE BLOOD PRESSURE OUTCOME **PREDICTION**

With cPWV, mAAD, mPWV and mTAC, four different markers of arterial stiffness were available to establish a prediction model. Of these, only mAAD and logarithmic mAAD were univariable predictors of 24h BP reduction. Individually, both were also independent predictors of 24h BP reduction at follow-up **(Table 2)**. Baseline 24h systolic BP, prescription of 5 or more drug classes as well as female gender were also identified as independent predictors for 24h systolic BP reduction. Serum creatinine and isolated systolic hypertension (ISH) were significantly associated with 24h systolic BP reduction upon univariable analysis but did not reach significance level in multivariable analysis **(Table 2)**.

Logarithmic mAAD had a poor but significant correlation with 24h systolic BP (r^2 =0.150, p <0.001) and had an acceptable

accuracy in predicting 24h BBPR after 3 months (AUC 0.714). Using an OST (-5.2) to detect 24h BBPR as described above, a significantly stronger systolic and diastolic BP reduction was found in patients with mAAD below, in comparison to patients above, the OST $(p<0.05$ for both, systolic and diastolic BP). Resulting 24h BBPR frequencies in the 2 groups were 65% and 31% **(Figure 3)**.

A multivariable model including logarithmic mAAD and all independent predictors as stated above, showed a modest correlation with systolic 24h BP change after 3 months ($r^2=0.427$, $p<0.001$) and had an acceptable accuracy in predicting BBPR (AUC 0.791). Using an OST (-5.0), a significantly stronger systolic and diastolic BP reduction was observed in patients below versus above OST $(p<0.001$ for both). BBPR frequencies in the 2 groups were 72% and 24% **(Figure 3)**. Upon logistic regression, baseline systolic 24h BP, logarithmic mAAD and intake of 5 or more drug classes were independent predictors of BBPR, while female gender was not **(Supplementary Table 3)**. Upon penalised regression analysis for systolic 24h BP reduction, only baseline systolic 24h BP and logarithmic mAAD contributed significantly to the model (Beta=-0.204 and -0.244, p=0.05 and 0.006, respectively, regularised r²=0.334) **(Table 2)**.

A bivariable model including 24h systolic baseline BP and logarithmic mAAD was significantly correlated with systolic 24h BP change (r^2 =0.270, p <0.001) and yielded an AUC for BBPR prediction of 0.740. Using an OST (-5.0), BP reduction was more pronounced in patients below versus above OST (p<0.001 for both), and corresponding BBPR rates were 69 and 38% **(Figure 3)**. Upon logistic regression, logarithmic mAAD was an independent predictor of BBPR $(p=0.002)$.

The cut-off values for OST as well as regression equations for each model are presented in **Supplementary Table 4**. Correlations between the individual measures of arterial stiffness are presented in **Supplementary Table 5**.

COMPARISON WITH iPWV

AUCs for BBPR prediction did not differ significantly between logarithmic mAAD, the bivariable and the multivariable model in comparison to iPWV (AUC 0.714, 0.740 and 0.791 vs 0.695, p=n.s. for all). The bivarible and the multivariable model were significantly better correlated with 24h systolic BP change after 3 months than iPWV alone (r^2 =0.427 and 0.270 vs 0.055, p<0.001 and p=0.04 respectively), while logarithmic mAAD was not $(r^2=0.150, p=0.31)$.

VALIDATION

Fifty-two patients were available for validation. Mean 24h systolic and diastolic BP were reduced by -5.4 ± 11.0 and -4.4 ± 7.7 mmHg ($p<0.001$). 24h BBPR was observed in 33 patients (63%). In the validation cohort, logarithmic mAAD and 24h systolic baseline BP were confirmed as independent predictors upon linear regression analysis, while female gender and prescription of 5 or more antihypertensive drug classes were not **(Supplementary Table 6)**. Correlation coefficients did not differ significantly between the 2 study cohorts for logarithmic mAAD and the bivariable model $(r^2=0.118 \text{ vs } 0.150 \text{ and } 0.304 \text{ vs } 0.270, p=0.80 \text{ and } 0.76)$ but were significantly lower for the multivariable model in the validation cohort (r^{2=0.149} vs 0.427, p=0.04).

Application of the OST values for predicted non-response from the exploratory analysis showed a significant reduction of 24h systolic BP in patients below versus above OST for logarithmic mAAD and the bivariable model (p=0.03 and 0.04) **(Figure 4)** while BP was not different between the groups when using the multivariable model.

Application of a Youden index-based threshold instead of OST showed similar results, with significant BP difference between the groups for mAAD and the bivariable model and no significant difference for the multivariable model, but the group with a low likelihood for BP reduction at follow-up expanded to roughly 50% of patients with all 3 models.

Table 2. Exploratory outcome – uni- and multivariable linear as well as penalised regression for 24h blood pressure reduction after 3 months. Data presented for non-invasive markers of arterial stiffness as well as for significant (univariable) clinical variables.

PWV: pulse wave velocity

Figure 3. *Exploratory outcome. Accuracy of predicted blood pressure change 3 months after RDN (left column) and prediction of a binary blood pressure response >5 mmHg (mid column) for invasive pulse wave velocity, ascending aortic distensibility, a multi- and a bivariate model. Systolic (blue) and diastolic (green) blood pressure change and 24 hr binary blood pressure responder frequencies using the predefined cut-off for iPWV and optimal sensitivity thresholds for ascending aortic distensibility, the bi- and the multivariate models (right column). *p<0.05; **p<0.001. Error bars indicate 95% confidence intervals. AUC: area under the curve; iPWV: invasive pulse wave velocity; mAAD: ascending aortic distensibility; OST: optimal sensitivity threshold; RDN: renal denervation; ROC: receiver operator characteristics*

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Discussion

This trial is the first to prospectively confirm a predefined, independent predictor for BP reduction following RDN. Secondly, this is the first systematic prospective evaluation of a) clinical predictors, b) invasive, and c) non-invasive assessment of arterial stiffness as predictors for RDN success in a single trial. With these analyses, we were able to develop a validated, non-invasive prediction model for RDN success.

Our findings confirm the key role of arterial stiffening in the BP response to sympathetic nervous system modulation following endovascular RDN. Arterial stiffening has long been thought to be a major contributor to the endemic clinical problem of arterial hypertension¹⁶. Regarding RDN, it has been suggested as a potential treatment target¹⁷, but also as a predictor of RDN response. The latter is important, since an accurate and clinically applicable predictor of RDN response prior to the procedure is currently an unmet need.

As the accepted reference standard for arterial stiffness estimation, an elevated iPWV is usually associated with advanced vascular remodelling and loss of elastic cushioning function $13,18$. It is also associated with increased pulse pressure and age^{18,19}. In contrast, renal norepinephrine spillover as a marker for renal sympathetic activity (the therapeutic target of RDN) is elevated in patients with essential and resistant hypertension^{20,21} but seems to reduce with age²². Thus, in patients with exceedingly high iPWV, the contribution of sympathetic activity to BP elevation might be diminished. Instead, the contribution of biomechanical components to hypertension predominates, which makes BP reduction after RDN less likely. This concept is supported by our previous studies⁸⁻¹¹ and various other trials identifying different markers of vascular stiffening and ageing as negative predictors for BP reduction after RDN23-25.

While accumulating data points towards iPWV as an independent predictor of RDN success, its invasive nature hinders its practical application in the general RDN population. We therefore investigated the potential of 2 non-invasive approaches to estimate arterial stiffness and consequently response to RDN: estimation of cPWV and an MRI-based model. Of all the markers assessed, only mAAD was independently associated with overall BP changes and confirmed in the validation study.

Contrasting our results on iPWV, using cPWV to identify patients with a low likelihood for BP change was futile. We also found a low correlation only between iPWV and cPWV. Besides measurement inaccuracies, this might be explained by the algorithm of the specific device, Complior, which tends to underestimate pulse wave velocity at higher levels of iPWV12. As mean and median iPWV were at very high levels in this study, the predictive accuracy of cPWV might have been hampered. Nevertheless, evaluation of other devices for cPWV estimation to predict BP change might be a worthwhile effort, as the use of a bedside tool could be more cost effective than MRI.

mPWV and mTAC also failed to precisely detect non-responders and to predict the extent of BP reduction at follow-up. This might be explained by the different methodology used for mPWV, which uses flow curves instead of pressure waves. Even though flow usually follows pressure increase, this could lead to a loss of precision in its accuracy when compared to iPWV. MTAC is only a very broad estimate of arterial stiffness and was numerically less precise than mAAD and iPWV in predicting BP change after RDN in one of our previous publications¹¹. Altogether, both measures apparently lack the precision necessary to predict BP reduction after RDN.

The multivariable model was inaccurate in the validation cohort. This can be explained by a chance finding in our study cohort: improved BP reduction in women, and a lesser BP reduction in patients prescribed 5 or more antihypertensive drugs have never been described for RDN patients before, even in the large-scaled Global Symplicity Registry²⁶. A device-specific factor for endovascular ultrasound RDN leading to this observation cannot be excluded here, but pathophysiologic assumptions make this explanation less likely. It might be an option to revalidate this model in an ultrasound RDN cohort in the future, but until then the multivariable model described here is not applicable in practice.

The bivariable mAAD-based model and logarithmic mAAD alone were the only non-invasive models predictive for RDN response, which remained significant after multivariable analysis and validation in a second study cohort. MAAD represents the central cushioning elements of the vasculature, which might give

Figure 4. *Validation of non-invasive prediction models – 24h systolic (blue bars) and diastolic (green bars) blood pressure change after 3 months, dichotomised by the optimal sensitivity threshold from the exploratory analysis for (A) ascending aortic distensibility, (B) the bivariable model and (C) the multivariable model. *p<0.05; n.s.: not significant. Error bars indicate 95% confidence intervals. OST: optimal sensitivity threshold*

a more accurate estimation of vascular and biomechanical contribution to BP composition than iPWV, even though pulse wave velocity is regarded as the gold standard for arterial stiffness assessment¹³. In our previous study on prediction of BP response after RDN, mAAD was the only predictor with a numerically higher AUC than $iPWV^{11}$, which is in line with the findings presented herein.

Even though MRI is cost-intensive, and its availability is limited, its use is often indicated or necessary in patients with treatment-resistant hypertension to exclude renovascular hypertension, as recommended by current guidelines, although this is usually a domain of duplex sonography^{1,27}. It also facilitates RDN by identifying accessory arteries and potential access site-related pitfalls. In this setting, additional sequences to assess vascular stiffness before RDN could be performed with minimal extra cost and effort but yield important supplementary information.

Overall correlations between the prediction models and systolic BP changes might seem poor, but their practical implication is more significant: application of cut-off values for mAAD and the bivariable model leads to an exclusion of roughly 1/5 (mAAD) and 1/3 (bivariable) of patients with low pretest probability to RDN and only few potential BP responders among them. This allows minimisation of futile interventions in these patients who are the least likely to respond – an important advance in a population of resistant and refractory hypertensive patients, where prediction of BP response is often blurred by comorbidities and fluctuations in medication adherence3,28.

Of course, application of these models should not lead to general preclusion of patients with low pretest probability for success from RDN, but it could be a useful tool for shared decision-making between patients and practitioners and support a patient-preference centred treatment strategy.

The bivariable model is somewhat prone to regression to the mean, as it includes baseline systolic BP as a variable. Elevated baseline systolic BP repeatedly has been described as a strong predictor for RDN success^{8,25,26}. This could be explained by regression to the mean, but elevated BP could also represent a higher level of sympathetic activity and thus explain the improved responsiveness in these patients.

Limitations

Several limitations need to be mentioned. First, this is a singlecentre trial in a highly specialised centre, which hinders generalisation of its results. Second, overall responder rates are lower than in recently published RDN trials²⁻⁴. This could be explained by a different trial population with more severe hypertension and intensified medical co-treatment. When compared to patients from the Global Symplicity Registry, who were on a similar level of antihypertensive treatment and had similar comorbidities, responder rates are similar²⁶. Third, we cannot provide drug adherence testing for the patients enrolled. Poor drug adherence is a well-known problem in patients with treatment resistant hypertension, even in RDN trials^{3,28}. Thus, results might differ when correcting for medication adherence or when conducting a trial in patients without

antihypertensive drug treatment. Fourth, the validation cohort was small, consisted of patients with radiofrequency RDN treatment only and had a lower overall BP reduction than the study cohort. Even though this could also be interpreted in favour of the robustness of our findings for the bivariate model and mAAD, confirmation in larger scaled studies is warranted. Fifth, we did not include a control group in this trial. Thus, we cannot fully exclude that similar BP changes would occur without RDN spontaneously.

Conclusions

This trial confirms the predictive value of iPWV for BP reduction after RDN. It also supports the use of mAAD and a bivariable model, based on mAAD and baseline BP, as predictors for RDN response. The improvement in responder rates resulting from these models when applied to patients before RDN could facilitate trial design and change clinical decision-making in the future. Consequently, they could enhance the relevance of RDN as a treatment option in high-risk treatment-resistant hypertension patients in daily clinical practice.

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Impact on daily practice

For the first time in a prospective study, arterial stiffness is confirmed as a predictor of blood pressure reduction after renal denervation (RDN). Also, non-invasive prediction of this blood pressure response is feasible. Application of invasive and noninvasive prediction models for blood pressure outcome after interventional renal denervation could facilitate patient selection for future RDN trials as well as clinical decision-making.

Conflict of interest statement

P. Lurz and K. Fengler received modest institutional fees from ReCor Medical and Medtronic. The other authors have no conflicts of interest to declare.

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Supplementary data

Supplementary Appendix 1. Methods: study participants, validation cohort, blood pressure measurement, measurement of invasive pulse wave velocity, anatomic assessment and exclusion of secondary hypertension, MRI specifications, sample size, regression models and other statistics.

Supplementary Appendix 2. Results: medication adherence.

Supplementary Table 1. Baseline characteristics in patients below the prespecified iPWV cut-off or above.

Supplementary Table 2. Primary outcome – multivariable linear regression for (A) daytime blood pressure reduction after 3 months and (B) 24h blood pressure reduction after 3 months.

Supplementary Table 3. Logistic regression analysis for the multivariate model.

Supplementary Table 4. Regression equations and optimal sensitivity thresholds.

Supplementary Table 5. Linear correlation coefficients (Pearson) between different markers of vascular stiffness.

Supplementary Table 6. Validation – uni- and multivariable linear regression for 24h blood pressure reduction after 3 months in the validation cohort.

Supplementary Table 7. Blood pressure and heart rate during assessment of vascular stiffness.

[The supplementary data are published online at:](https://eurointervention.pcronline.com/doi/10.4244/EIJ-D-21-01036) https://eurointervention.pcronline.com/ doi/10.4244/EIJ-D-21-01036

Supplementary data Supplementary Appendix 1. Methods

Study participants

To provide optimal adherence, the patients' general practitioners were contacted and asked whether trial participation was supported and whether the patient was considered adherent to medication. Patients without sufficient medication adherence, by general practitioner report, were excluded.

Only patients with data from all 3 methods for arterial stiffness estimation (invasive, MRI and bedside pulse wave velocity) were included in the study. Patients were blinded to all results related to vascular stiffness testing.

Validation cohort

The external validation cohort consisted of patients from a prospective trial on different RDN techniques, which used comparable in- and exclusion parameters and in which patients underwent the same assessment of arterial stiffness. Only patients with full MRI and clinical dataset were included in the validation cohort. Altogether, 52 patients were available for validation.

Blood pressure measurement

Screening office BP was measured with automated BP monitors (Omron M300; Omron Healthcare and Boso medicus uno; Boso) from a single measurement in sitting position after 5 min. of rest (attended BP measurement). ABPM was acquired with a cuff-based oscillometric device (Spacelabs model 90207; Spacelabs Healthcare), adapted to patient's arm circumference. BP recordings were registered every 15 minutes during daytime (7:00 AM-10:00 PM) and every 30 minutes during night-time (10:00 PM-7:00 AM).

Measurement of invasive pulse wave velocity

IPWV was calculated according to the following equation: v=pigtail-length [m]/(foot-to-foot distance [m]/recording speed [m/sec]), Pigtail-length measured between the first hole of the distal part and its entry into the distal end of the sheath.

Anatomic assessment and exclusion of secondary hypertension

Patients underwent MRI for the assessment of renal artery anatomy and exclusion of renal artery stenosis. All patients were screened for hyperaldosteronism prior to study inclusion (by lab testing for aldosterone-to-renin ratio) and if pathological results were detected, were precluded from the study and referred to an endocrinologist. Screening for obstructive sleep apnoea was prompted if patient's history was suspicious for sleep apnoea (excessive tiredness during the daytime, snoring or observed apnoea by partners) or if ABPM showed an inverse dipping pattern. Other secondary causes of arterial hypertension were excluded as appropriate.

MRI specifications

Scans were performed on Siemens 3T scanners (Verio; Siemens Healthineers,). MRI analyses were performed by investigators blinded to patient's baseline characteristics and outcome.

Aortic area measurements were performed using OsiriX open-source software (OsiriX 5.7). Aortic flow measurements were acquired from phase contrast imaging and left ventricular stroke volume (SV) determined by integrating the aortic forward flow. Aortic flow and aortic pulse wave velocity were assessed using Segment 4.5.0 (Medviso AB).

Simultaneous non-invasive BP measurements during flow measurements (conventional automated arm-cuff based measurement, average from three single recordings) were used to calculate total arterial compliance (mTAC) and ascending aortic distensibility (mAAD).

Total arterial compliance

mTAC was calculated using stroke volume (SV) derived from forward flow and simultaneous measurements of non-invasive pulse pressure (PP) according to the formula mTAC=SV/PP.

Ascending aortic distensibility

Minimum and maximum ascending aortic cross-sectional areas were acquired distal to the aortic bulbus at pulmonary artery bifurcation level, perpendicular to the course of the ascending aorta, in cine steady state imaging.

mAAD was calculated as follows (Aomin=minimal cross-sectional aortic area, Aomax=maximum crosssectional area, PP=non-invasive pulse pressure): mAAD=(Aomax–Aomin)/(PPxAomin).

Magnetic resonance imaging pulse wave velocity

MRI-based pulse wave velocity (mPWV) was measured using forward flow from the ascending aorta at the level of pulmonary artery bifurcation and from the descending aorta at diaphragm level.

Sample size

We hypothesised a mean BP change of 12 mmHg in a power systolic daytime BP on ABPM after 3 months in patients with low iPWV (<14.4 m/s) and a change of 4 mmHg in patients with high iPWV (\geq 14.4 m/s) as well as a standard deviation of 10 mmHg in both groups. To achieve of 90% at a two-sided alpha level of 0.05, a sample size of 34 patients per group was required. To compensate for a potential loss to follow-up, total enrolment of 80 patients was planned.

Regression models

To confirm our previous finding on IPWV, univariable and stepwise multivariable linear regression analyses with systolic daytime BP reduction after 3 months as the dependent variable were performed including the following independent variables: IPWV, baseline systolic, diastolic and mean daytime BP, resting heart rate, presence of isolated systolic hypertension, age, sex, smoking status, diabetes, peripheral arterial disease, coronary artery disease, previous stroke or transient ischaemic attack, previous myocardial infarction, presence of heart failure symptoms, body mass index, baseline serum creatinine, all different classes of antihypertensive drugs, number of antihypertensive drug classes and intake of five or more drug classes. Only variables below a p-value of 0.05 in univariable analysis were included in the multivariable model by stepwise-forward selection. To address the prediction of general 24h BP reduction, an additional analysis was calculated, which included the same independent variables but systolic 24h BP instead of daytime BP as dependent variable. Linearity was tested using residuals vs fitted plots. Multicollinearity was tested by variance influence factor (with values <10 for all included variables, multicollinearity was refused).

To investigate the predictive value of the different non-invasive markers of arterial stiffness, univariable and stepwise multivariable linear regression analyses for prediction of systolic 24h BP change were calculated. The uni- and multivariable analyses included the same clinical variables as described above in addition with cPWV, mAAD, mTAC and mPWV instead of iPWV. MRI-based stiffness parameters and cPWV were analysed as absolute numbers as well as in a logarithmic form. Only variables below a p-value of 0.05 in univariable analysis were included in the multivariable model by stepwise-forward selection. To assess for overfitting, all confirmed independent predictors from this multivariable model were included into a penalised regression model (Elastic net) in an additional step with 24h BP change as the dependent variable.

In a last step, a bivariable linear regression model was calculated using baseline 24h systolic BP and logarithmic mAAD only.

To predict binary blood pressure response (BBPR), logistic regression analyses with BBPR as a dependent variable were conducted using only independent variables from the linear 24h BP change models. The models contained in detail: 1) baseline iPWV, baseline 24h systolic BP, intake of five or more drug classes as well as female gender for the invasive model; 2) logarithmic mAAD baseline 24h systolic BP, intake of five or more

drug classes as well as female gender for the multivariable model; and 3) logarithmic mAAD and baseline 24h systolic BP for the bivariable model.

Other statistics

Continuous variables are presented as mean and standard deviation, dichotomous variables as number and percentage unless indicated otherwise. Normal distribution was tested using Kolmogorov-Smirnov tests. Student's t-tests or Mann-Whitney U tests were used to compare continuous variables. Chi-square tests were used to compare dichotomous variables.

Linear correlation coefficients were compared using Fisher's z-transformation. The underlying assumptions of the statistical tests were evaluated. Statistical significance was inferred when $p<0.05$.

Supplementary Appendix 2. Results: medication adherence

Medication was changed in 13 patients between RDN and follow-up (reduced in 10, increased in 3 patients). When analysing patients on stable medication only, results for the primary outcome remained significant (p<0.05) and correlations to blood pressure change for the different prediction models were similar to the results for the full cohort (r² for logarithmic iPWV, mAAD. the multivariable and the bivariable model=0.04, 0.10, 0.58 and 0.33, respectively).

Supplementary Table 1. Baseline characteristics in patients below the prespecified iPWV cut-off or above.

Supplementary Table 2. Primary outcome – multivariable linear regression for (A) daytime blood

CI: confidence interval; iPWV: invasive pulse wave velocity; ISH: isolated systolic hypertension; n.s: not significant.

Supplementary Table 3. Logistic regression analysis for the multivariate model.

Supplementary Table 4. Regression equations and optimal sensitivity thresholds.

24h SBP: 24h ambulatory systolic blood pressure; drugs: prescription of 5 or more antihypertensive drug classes (yes=1, no=0); female: female gender (yes=1, no=0); mAAD: ascending aortic distensibility.

	Invasive	Ascending	Transformed	Total arterial	Magnetic-	Carotid-
	PWV	aortic	PWV from	compliance	resonance-	femoral
		distensibility	distensibility		imaging	PWV
					PWV	
Invasive PWV	$\mathbf X$	-0.419	0.436	-0.303	0.214	0.221
Ascending aortic	0.419	\mathbf{X}	-0.801	0.401	-0.274	-0.255
distensibility						
Transformed PWV	0.436	-0.801	$\mathbf X$	-0.469	0.392	0.331
from distensibility						
Total arterial	-0.303	0.401	-0.469	$\mathbf X$	-0.411	-0.219
compliance						
Magnetic-	0.214	-0.274	0.392	-0.411	\mathbf{X}	0.169
resonance-imaging						
PWV						
Carotid-femoral	0.221	-0.255	0.331	-0.219	0.169	$\mathbf x$
PWV						

Supplementary Table 5. Linear correlation coefficients (Pearson) between different markers of vascular stiffness.

Supplementary Table 6. Validation – uni- and multivariable linear regression for 24h blood pressure reduction after 3 months in the validation cohort.

classes

*: when included instead of logarithmic ascending aortic distensibility.

CI: confidence interval; n.s: not significant.

Supplementary Table 7. Blood pressure and heart rate during assessment of vascular stiffness.